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Integrative computed tomographic imaging of coronary artery disease

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Rapid technological evolution in multislice computed tomography (CT) over the last decade with improved spatial and temporal resolution has enabled cardiac CT to become a viable and effective alternative in the diagnosis of coronary artery disease. Within recent years CT coronary angiography has demonstrated high sensitivity and specificity, and in particular a very high negative-predictive value, making it a valuable imaging modality for ruling out suspected coronary artery disease. In addition, CT angiography demonstrates accuracy in the detection and characterization of coronary plaques, and it has been reported to play an important role in predicting disease progression and cardiac events. The goal of this article is to provide an overview on the role and current clinical applications of cardiac CT in the evaluation of coronary artery disease. Emerging areas of cardiac CT, including dual-energy CT and CT myocardial perfusion are also discussed, as well as the limitations and future directions of cardiac CT.

KEYWORDS: cardiac computed tomography • coronary artery disease • dual-energy computed tomography • dual-source computed tomography • myocardial perfusion computed tomography

Coronary artery disease (CAD) represents the most relevant cause of death and morbidity in the adult population of developed and developing countries [1,2]. During the last decades, strong research and financial effort has been made to identify more selective biomarkers and refine imaging technologies to better assess the cardiovascular risk in both primary and secondary prevention [3].

Rapid technological advances have made computed tomography (CT) a widely embraced modality in the non-invasive evaluation of CAD [4]. The capabilities of multidetector row CT (MDCT) to identify and rule out significant coronary artery stenosis have been consistently confirmed and clinically embraced as a core application of cardiac CT [5–13]. For comprehensive imaging of the heart, CT has been evaluated for the assessment of the myocardium, myocardial perfusion and viability, cardiac function, wall motion, as well as cardiac valves [14–20]. Nevertheless, the diagnostic value of cardiac CT beyond strict morphological evaluation of coronary stenosis remains uncertain. It proved to be surprisingly difficult to predict the hemodynamic relevance of stenosis and further stratify risk by detailed plaque characterization strictly based on anatomical information acquired during CT coronary angiography [21,22].

However, most recent advances in CT technology, including larger detector coverage and the availability of two generations of dual-source CT (DSCT) systems combined with substantial research efforts focused on plaque characterization and identification of positive remodeling suggest the feasibility of CT as a standalone modality allowing an integrative assessment of all aspects of coronary heart disease [23–26].

The purpose of this article is to review current and future applications of cardiac CT in the evaluation of CAD.

Technical evolution

In 1984, electron-beam CT was introduced as the first system capable of ECG-synchronized CT imaging of the cardiac anatomy [27]. The rapid rise of cardiac CT from a research application to a clinically appreciated modality was mainly driven by the introduction of MDCT. Since 1998, four-slice CT systems with higher volume coverage speed and improved temporal resolution of 250 ms have been clinically used for cardiac examinations at low to moderate heart rates, enabling quantification of coronary artery calcification and initial evaluation of coronary artery stenosis, cardiac function and the analysis of atherosclerotic plaque [28–33]. With each subsequent scanner

generation and improvement in temporal resolution, the proportion of successfully examined patients with non-invasive coronary CT angiography gradually increased [34]. The introduction of 64-slice CT systems in 2004 further increased temporal resolution up to approximately 165 ms, enabling detailed image acquisition of the heart with a 5–10 s scan time [35,36]. However, temporal resolution in patients with high heart rates and irregular heart rhythm was still limited, making pharmacological modulation for heart rates above 60–70 beats per minute (bpm) essential [37,38].

With the introduction of DSCT in 2006, a new scanner concept was presented consisting of two x-ray tubes and two detectors mounted perpendicularly in the same gantry [39]. This configuration allows full image reconstruction during quarter-rotation scanning as opposed to half-rotation scanning with conventional single-source multidetector CT systems, improving the temporal resolution to approximately 83 ms, reflecting one-quarter of the gantry rotation time [39,40]. With the recent introduction of second-generation DSCT, a 'high-pitch single-heartbeat acquisition' became feasible. In early reports, the ability of DSCT to perform ECG-triggered spiral data acquisition using very high pitch values (≥ 3.0) has been described. The application of high pitch values allows for an image acquisition of the entire volumetric data set of the heart within one cardiac cycle. As pitch is inversely related to radiation exposure, this scan mode is associated with approximately one-tenth of the exposure of a retrospectively ECG-triggered spiral scan and half to one-third of the dose of a prospectively ECG-triggered scan [41,42].

Motivated by the concept to completely cover the scanning volume within a single heart beat, 256- and 320-row single-source systems, as well as 128-row dual-source CT scanners, have been introduced recently [43,44]. The availability of detector arrays that are wide enough to cover the entire cardiac anatomy also enables new approaches in the assessment of cardiac function, including the acquisition of dynamic, time-resolved data on myocardial perfusion and the myocardial blood supply. These advancements may also reduce patient radiation and susceptibility to arrhythmia [43–45].

Furthermore, dual-energy acquisition techniques for the evaluation of myocardial blood supply based on static, non-time-resolved CT coronary angiograms using DSCT are being investigated [46,47]. Operated in dual-energy mode, the two-tube configuration of DSCT enables the simultaneous acquisition of high and low x-ray energy spectra with a single CT scan, permitting analysis of myocardial blood supply by determining the iodine (and thus blood) volume of the myocardium [46–48].

In addition, alternative image reconstruction approaches are being introduced that hold promise to realize substantial artifact and noise reduction, while at the same time increasing image sharpness, thus consequently increasing the accuracy of stenosis detection with coronary CT angiography, enabling a more precise delineation of calcified plaques and enhancing diagnostic capabilities to detect restenosis in coronary artery stents. The term 'iterative reconstruction' is used for a variety of approaches that either rely on ray-tracing in the image to calculate synthetic projections that are then compared with the originally measured projections to derive correction terms, or translate the iteration process into the image

domain by performing an iterative chain of locally adapted nonlinear image processing steps. Although increased spatial resolution is directly correlated with increased image noise in standard filtered backprojection reconstructions as they are used in CT scanners today, iterative reconstruction approaches to a certain extent allow the decoupling of spatial resolution and image noise. In an iterative reconstruction, a correction loop is introduced into the image reconstruction process. Iterative corrections are performed with further image noise reduction without degrading image sharpness, and involve a comparison of an initially reconstructed master image with a corrected image. Besides an increase in diagnostic accuracy, the decrease in image noise provided by iterative reconstruction allows for a significant reduction of radiation dose in routine clinical use while maintaining similar signal-to-noise ratios as with standard radiation dose acquisition protocols [49,50].

Coronary calcium scoring

Coronary calcium scoring using CT has been validated as a useful imaging tool for risk stratification and reclassification of the risk of CAD [51]. Atherosclerotic lesions of the coronary arteries often contain calcified components that used to be accurately measured by electron beam CT, but this method has been replaced by MDCT applying the Agatston scoring methodology [52,53]. Recent guidelines from the American Heart Association reviewed scientific data for cardiac multislice CT imaging of CAD and atherosclerosis in symptomatic and asymptomatic patients, and approved screening using calcium scoring as a methodology to reclassify risk in patients with an intermediate risk based on traditional scores such as the Framingham and Procam algorithms [54]. Further effort has been undertaken to correlate atherosclerosis to different pathological processes. One example is the Rule Out Myocardial Infarction Using Computer-Assisted Tomography (ROMICAT) trial, which sought to determine whether aortic valve calcification is associated with the presence and extent of the overall plaque burden, as well as with plaque composition. As a result it was suggested to consider aggressive medical therapy if aortic valve calcification was present [55].

Computed tomography calcium scoring is usually performed as a screening method in a low radiation dose scanning technique to detect and calculate the density, volume or mass of calcified plaques. The total coronary calcium burden is used for prognosis and risk stratification in CAD. The underlying rationale is the concept that coronary artery calcification is part of the atherosclerotic degeneration of the arterial wall, and coronary atherosclerosis is the only disease associated with calcium in the coronary arteries [56]. Thus, measurement of the amount of calcium allows for an accurate estimation of the amount of coronary atherosclerosis and, therefore, the risk of CAD. The total calcium score is calculated by adding up the volume of calcium in all coronary arteries by a weighting factor, dependent on the density of each calcified plaque. Calcium scoring is regarded as a good and independent predictor of cardiac events and adds incremental prognostic value to other risk factors [57,58]. Increasing degrees of coronary calcium scores predict adverse cardiovascular events and all-cause mortality [57,59–61].

Patients with a normal or zero calcium score fall into the lowest risk category, and are thus associated with a low risk of cardiac events, or are considered to be clinically absent of any major atherosclerosis [57,60,62]. The predictive value of this methodology has been further supported recently. In their study, Min *et al.* aimed to identify the incidence and predictors of conversion for a normal to abnormal coronary artery calcium score over a period of 5 years [59]. They concluded that the rate of conversion to an abnormal calcium score was nonlinear and occurred at a low frequency before 4 years of follow-up, suggesting that repeat calcium scoring examinations should not be performed for a minimum of 4 years in individuals with a normal calcium score of zero [59]. However, even though a negative calcium score is associated with a low risk for developing cardiovascular events in the following 2–5 years, it may not exclude luminal obstructive disease, especially in patients who are young and present with acute coronary syndrome [63–65]. Rubinshtein *et al.* concluded that 7% of patients with acute or long-term chest pain who had zero calcium score at CT were found to have significant CAD [66]. According to the literature the cumulative incidence of a zero or low calcium score is associated with a risk of 0.1 and 0.7% of cardiac events with a follow-up period of 3–5 years [52]. In addition, thickness of reconstructed slices is important as 3.0-mm or thicker slice reconstructions result in missing calcified lesions compared with 0.5-mm slice reconstructions [58,67].

Despite the recognized limitations of this test, coronary calcium scoring is currently seeing renewed interest as an aid for further cardiovascular risk stratification and risk factor management in both asymptomatic and symptomatic populations [51]. The technology is seen as an opportunity to non-invasively assess the progression of CAD and monitor the clinical efficacy of medical therapies by tracking the changing calcium score. As clinical decision making regarding the need for medical intervention can often be uncertain in asymptomatic individuals with one or more conventional risk factors for coronary disease, a technology such as coronary calcium scoring might become integral [68]. The importance of calcium scoring for clinical decision making was recently acknowledged by Polonsky *et al.* [69]. Their study demonstrated that adding calcium scoring to traditional risk factors results in a significant improvement in the classification of risk for the prediction of cardiovascular events in an asymptomatic population sample. They concluded that the use of calcium scoring plus traditional risk factors substantially enhances the ability to classify a multiethnic cohort of asymptomatic persons without known cardiovascular disease into clinically accepted categories of risk of future cardiovascular events.

To date, asymptomatic individuals with intermediate cardiovascular risk are seen as candidates for CT coronary calcium screening to allow improved risk stratification and to determine the level of aggressiveness of risk factor modification. In high-risk individuals the role of coronary calcium screening is still debated [54]. Further guidance can be expected with the upcoming update of the American College of Cardiology/American Heart Association recommendations. Nevertheless, additional integrating evidence regarding all available techniques is needed to determine the most practical and effective system for assessing cardiac risk to optimally target and follow the effect of preventive measures.

CT coronary angiography

Over the last decade, there has been increasing interest in the imaging and diagnosis of CAD using multislice CT owing to its non-invasive nature and fast scanning technique with extended z-axis coverage. Early studies using four-slice and 16-slice CT showed moderate diagnostic accuracy with pooled sensitivities and specificities of 78 and 93%, and 82 and 95%, respectively [28,35,68,70,71].

With the introduction of 64-slice CT and substantial improvements in spatial and temporal resolution, pooled estimates of assessable segments for CT coronary angiography increased to 97%, assessable segments were found to improve with the increase of CT detectors and significant difference was reached comparing 64-slice with four- and 16-slice scanners [71]. In the Assessment by Coronary Computed Tomographic Angiography of Individuals Undergoing Invasive Coronary Angiography (ACCURACY) prospective multicenter study of patients with chest pain without known CAD and intermediate disease prevalence, 64-slice CT angiography had a patient-based sensitivity of 94% and specificity of 83% in detecting coronary stenosis of 70% or more [72]. In the Coronary Artery Evaluation Using 64-Row Multidetector Computed Tomography Angiography (CORE-64) prospective multicenter study of patients with suspected symptomatic CAD, 64-slice CT angiography had a patient-based sensitivity of 85% and specificity of 90% for detecting coronary stenosis of 50% or higher [73]. However, in both studies patients with heavy coronary artery calcifications were excluded. Other representative studies evaluating the performance of 64-row CT and DSCT for detecting hemodynamically significant coronary artery stenosis report sensitivities between 86 and 99%, specificities between 92 and 98%, positive-predictive values between 47 and 91%, and most importantly negative-predictive values between 92 and 100%, allowing a reliable non-invasive exclusion of significant coronary artery stenosis using CT [11,21,38,74–77]. The predictive value of this methodology has been further supported recently. In their study, Min *et al.* aimed to investigate the prognostic value of CT coronary angiography for the prediction of major adverse cardiovascular events [78]. They concluded that the CT coronary angiography presentation of plaque severity and composition successfully identifies patients at risk for major adverse cardiovascular events and a negative CT scan portends an extremely low risk for incidence of such events. TABLE 1 provides a further overview of recent literature. Nevertheless, despite the rapid advances in scanner technology and image postprocessing, at times motion artifacts from high or irregular heart rates, excessive image noise in obese patients, and heavy vascular calcifications, especially with calcium scores above 400, result in limited diagnostic accuracy [56,79–81]. Further improvements in scanner technology suggest improvements in image robustness, especially in high and arrhythmic heart rates, the ability to evaluate heavily calcified vessels, and reduced blooming artifacts from heavy calcification and metallic stents using dual-energy [82–84].

Currently, however, besides heavy calcifications of coronary arteries motion artifacts remain the most important challenge for coronary CT angiography even with the latest generation of scanners making further evaluation in symptomatic yet inconclusive

Table 1. Accuracy of 16-slice, 64-slice, 256-slice, 320-slice and dual-source computed tomography for the detection of coronary artery stenosis in comparison with invasive cardiac catheterization.

Author	Patients (n)	Sensitivity (%)	Specificity (%)	NPV (%)	PPV (%)	Ref.
16-slice CT						
Kuettner <i>et al.</i>	124	85	98	96	87	[191]
Mollet <i>et al.</i>	51	95	98	99	79	[192]
Hoffmann <i>et al.</i>	103	95	98	99	87	[193]
Achenbach <i>et al.</i>	50	94	96	99	69	[194]
64-slice CT						
Leschka <i>et al.</i>	53	94	97	99	87	[76]
Raff <i>et al.</i>	70	86	95	98	66	[80]
Leber <i>et al.</i>	59	88	97	99		[132]
Nikolaou <i>et al.</i>	72	86	95	97	72	[195]
256-slice CT						
Korosoglou <i>et al.</i>	27	86	95	90		[153]
Chao <i>et al.</i>	104	98.8	50	92.4	87.5	[196]
320-slice CT						
Dewey <i>et al.</i>	30	100	94			[197]
de Graaf <i>et al.</i>	64	94	95	88	98	[198]
DSCT						
Leber <i>et al.</i>	88	94	99	81	99	[11]
Johnson <i>et al.</i>	35	88	98	78	99	[199]
Ropers <i>et al.</i>	100	92	97	68	99	[77]
Brodoefel <i>et al.</i>	100	91	92	75	97	[200]

CT: Computed tomography; DSCT: Dual-source computed tomography; NPV: Negative-predictive value; PPV: Positive-predictive value.

patients necessary. In these patients additional non-invasive physiologic testing including nuclear myocardial perfusion imaging is recommended to identify intermediate but hemodynamically relevant stenosis [85].

In order to facilitate image interpretation and ensure diagnostic accuracy of stenosis identification, automated computer-aided detection solutions have recently been introduced (FIGURE 1). A recent study investigating the performance of a computer-aided detection algorithm for automated detection of significant stenosis at CT coronary angiography reported 100% sensitivity, 65% specificity, 76% accuracy, 100% negative-predictive value and 58% positive-predictive value compared with invasive cardiac catheterization [86].

To further guide referring physicians and radiologists in the use of this examination, the issuance of guidelines and appropriateness criteria by the professional societies has helped to define the indications for coronary CT angiography. There is consensus that coronary CT angiography is appropriate in symptomatic individuals, especially if symptoms, sex and age suggest a low-to-intermediate probability of significant coronary artery stenosis. There is also consensus that coronary CT angiography to date has

no role for general screening for coronary atherosclerosis in asymptomatic individuals with low and intermediate cardiac risk (class III, level of evidence C), because the current levels of radiation are incompatible with the prerequisites of a successful screening test and data on the cost-effectiveness of this indication are lacking [54,87–93]. Whether CT coronary angiography has incremental value for risk stratification, risk modification and therapeutic monitoring in asymptomatic high-risk individuals is a topic of ongoing research [94].

CT angiography of coronary artery bypass grafts

Invasive coronary angiography has been seen as the diagnostic standard for evaluating the status of both arterial and venous coronary artery bypass graft (CABG) vessels. However, CT has emerged as a promising non-invasive technique to visualize the coronary artery lumen and patency of the venous and arterial conduits. The anatomical features of arterial and vein grafts render these vessels specifically suitable for study with CT [95,96]. Because of their large size, relative immobility and lack of calcification, grafts appear ideally suited for evaluation compared with native coronary arteries [97]. While this applies mostly to venous grafts, arterial grafts (e.g., internal mammary arteries) can be more challenging to evaluate due to their smaller vessel diameter and more frequent artifacts caused by metallic

clips. Onuma *et al.* described limited evaluability of arterial grafts (90%) compared with venous grafts (99%) [98]. Recent studies comparing 16- and 64-slice CT with conventional coronary angiography describe sensitivities, specificities, positive and negative-predictive values up to 100, 95, 85 and 100%, respectively [98–100]. However, with sensitivities and specificities to detect significant stenoses as low as 83.3 and 80.2%, and up to 16% of distal run-offs nonassessable, evaluating the distal anastomosis and run-off arteries still remains challenging and might limit further clinical implementation [98,99,101]. Even though current data suggest attractive diagnostic potential in patients before or after cardiac surgery, the exact role of technological advances including DSCT in the exact evaluation of distal run-off vessels and anastomoses remains unclear and warrants further studies [102].

Coronary artery stents

Percutaneous coronary intervention and stent placement is a preferred method for minimally invasive coronary reperfusion. However, even with the advent of drug-eluting stents that are engineered to reduce the cellular proliferation that results in

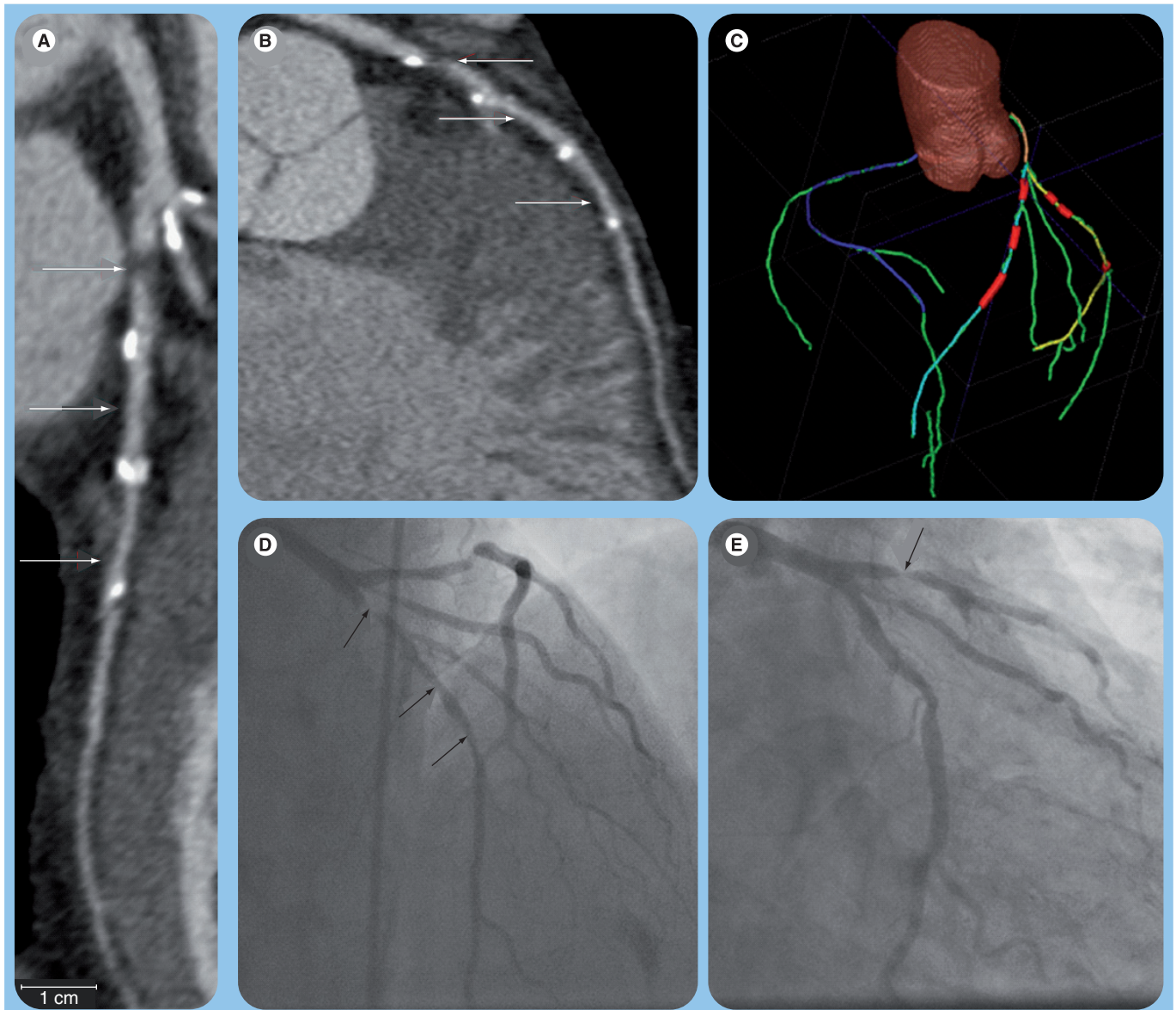


Figure 1. A 52-year-old man with a history of hyperlipidemia. (A & B) Curved multiplanar reformation of the left anterior descending artery and left circumflex artery shows several calcified and noncalcified plaques and stenoses (arrows). **(C)** Corresponding 3D segmentation by computer-aided detection algorithm, resulting in correct automated placement of detection markers. **(D & E)** Revealed stenoses were confirmed by invasive coronary catheterization.

neointimal hyperplasia, restenosis remains a common clinical problem, making early identification of crucial interest to prevent myocardial ischemia and improve prognosis [103].

Non-invasive assessment of coronary artery stent patency and detection of in-stent restenosis have been thoroughly investigated since the introduction of cardiac MDCT [104,105]. In clinical practice, stent patency is often determined by the visualization of contrast agent distal to the stent. However, patency can also be mimicked by collateral flow or retrograde filling. Conversely, the absence of contrast agent distal to the stent indicates severe in-stent restenosis [105]. The biggest challenge for MDCT technology is to overcome beam-hardening artifacts due to the stent's metallic composition and partial volume artifacts. With earlier

scanner generations lumen assessment was often not possible due to artifacts and sensitivities remained low [106,107]. Stent assessment using 64-slice MDCT has provided further improvements; however, stent size, type and metallic composition still greatly influence diagnostic visualization [108].

A meta-analysis by Hamon *et al.* reviewed the role of MDCT in 15 studies including 807 patients and 1175 stents [109]. The results demonstrated a pooled sensitivity of 85% and a specificity of 91% for 64-slice CT. However, in these 15 studies 13% of stents were excluded from evaluation, which potentially overestimates the performance of MDCT, leading the authors to conclude that the clinical use of MDCT as an alternative to invasive catheterization for in-stent restenosis detection remains limited.

To date, there are only a few studies investigating the role of advanced scanner generations for the evaluation of stent patency. In their study Pugliese *et al.* showed a sensitivity, specificity, positive-predictive value and negative-predictive value of DSCT of 94, 92, 77 and 98%, respectively [110]. However, performance of DSCT is hampered by frequent false-positive findings in smaller stents (≤ 2.75 mm). Furthermore, Oncel *et al.* demonstrated sensitivity, specificity and positive and negative-predictive values of DSCT in the detection of in-stent restenosis or occlusion of 100, 94, 89 and 100%, respectively [111]. In their population only two out of 48 stents (4.2%) were misclassified as stenotic and later proven patent at conventional catheterization. Initial results with 320-slice CT show that CT angiography allows accurate non-invasive assessment of significant in-stent restenosis with sensitivity, specificity, positive and negative-predictive values of 100, 81, 58 and 100%, respectively, on a patient basis [9]. Besides quite promising results using newest scanner generations, the diagnostic performance of CT is mainly influenced by stent type, stent diameter and thickness of stents struts [112]. Based on these results, invasive catheter angiography remains the gold standard for the assessment of coronary in-stent restenosis [9,112]. Further studies performed with newer scanner generations should focus on improving imaging techniques to reduce artifacts resulting from the implanted stents.

New & emerging applications

Cardiac function

Left ventricular volumes and function are predictive markers of a variety of cardiovascular diseases, and left ventricular hypertrophy is an important prognostic marker in patients with or without CAD. In addition, patients with both CAD and depressed left ventricular function are at high risk for sudden death [113–116]. While transthoracic and transesophageal echocardiography are applied routinely and radionuclide ventriculography has been used, MRI has evolved into the preferred technique for the exact determination of cardiac function parameters [117–119]. However, with advances in CT scanner technology and the existence of isotropic voxels, image reconstruction can be performed in any desired plane [120]. Despite early reports about the underestimation of left ventricular ejection fraction, visual evaluation of wall motion abnormalities detected at cardiac CT showed good agreement with echocardiography and MRI, and further improved with current scanner generations [120–126].

Results obtained with modern CT scanner generations starting with 64-slice CT approach the accuracy of cardiac MRI, with a slight overestimation of end-systolic volume compared with MRI, resulting in a systematic underestimation of left ventricular ejection fraction that ranges from 1 to 7% [117,119,120,123,127,128].

Nevertheless, each time retrospectively ECG-gated cardiac CT is performed, data inherently contain image information of the complete cardiac cycle, which can be used to evaluate ventricular wall motion and global functional parameters for additional diagnostic benefit. With the introduction of modern postprocessing software, intuitive analysis of cine images and immediate quantification of functional parameters can be achieved, making

the assessment of myocardial and valvular function an integrative part of the image interpretation for a comprehensive cardiac analysis [118,120,129].

Coronary atherosclerotic plaque imaging

Since it has been shown that contrast-enhanced CT coronary angiography can sensitively detect coronary atherosclerotic plaques and differentiate between calcified and noncalcified atherosclerotic plaque components, there has been intense interest in the evaluation of coronary CT angiography as a tool for risk stratification and for monitoring risk factors [130–132]. The underlying rationale is a growing understanding of the relationship between plaque composition and different clinical manifestations of CAD. Symptoms of chronic stable angina correlate well with stenotic, mainly fibro-calcified lesions, whereas acute coronary syndrome and sudden cardiac death are more likely to be associated with a rupture of previously nonstenotic, mostly lipid-rich, 'vulnerable' plaques [133–135]. Thrombus formation and plaque rupture play key roles in the onset of acute coronary syndrome. Plaque rupture is the most frequent cause of acute myocardial infarction and it has been recognized that thin-cap fibroatheroma (TCFA) is the primary plaque type at the site of plaque rupture [136–138]. With the hope of guiding patient management, coronary artery plaque composition has been extensively studied using invasive imaging techniques such as intravascular ultrasound and, more recently, optical coherence tomography [139–141]. However, the complexity, associated costs, invasiveness and restricted availability limit a more extensive clinical application of these modalities beyond specific clinical scenarios and research. To overcome some of these hurdles, CT coronary angiography, with its high temporal and spatial resolution, has been the subject of research to investigate the potential of an attenuation-based plaque detection and characterization. Studies have shown that CT is able to analyze coronary plaques quantitatively and qualitatively, especially by assessing the intraplaque density, and it has been shown that CT results correlate reasonably well with histological findings [142–147]. However, a direct comparison of intravascular ultrasound and multislice CT has revealed a general overestimation on multislice CT for quantitative measurements of all areas and thickness [132,148]. The formation of noncalcified plaque is recognized to be frequently associated with positive vascular remodeling, which is detectable on CT. Noncalcified plaques have CT attenuation values between 7 and 152 Hounsfield units (HU) and can be differentiated from epicardial fat (~ 30 HU) and unenhanced blood (~ 40 HU) [130,144,146]. On the basis of *ex vivo* studies, attenuation ranges for specific plaque components according to their HU have been proposed and MDCT has been cited to be able to identify differences in plaque morphologies between TCFA and non-TCFA [137,149]. However, *in vivo* attenuation measurements of coronary artery plaques are complicated by the small size and irregular shapes of target lesions resulting in substantial volume averaging, by substantial overlap in attenuation values of fibrous and lipid-rich plaques, and perturbing influences of contrast attenuation in the adjacent coronary lumen limiting a reliable differentiation beyond a characterization of calcified from noncalcified plaque components [150]. Because of increasing interest

in non-invasive atherosclerotic plaque characterization, a multitude of software solutions have been developed (FIGURE 2) allowing automated plaque detection and volumetric quantification of calcified and noncalcified atherosclerotic plaque components. Even though the accuracy and precision of these software applications remains largely unverified, they might have the potential to overcome limitations such as underestimation of mixed and noncalcified plaque volumes and a trend to overestimate calcified plaque volumes [143]. Despite promising results, the CT differentiation of lipid-rich content from fibrous content remains challenging due to considerable overlap in the attenuation values of lipid and fibrous tissues, leaving the identification of the truly 'vulnerable' plaque at risk of rupture a technological challenge and questioning the current clinical application beyond mere research [151].

Innovations in CT technology are promising to further enhance the ability of CT in the quantitative analysis of coronary plaques, but their role for a substantial improvement of coronary atherosclerotic plaque characterization in a clinical setting still needs to be evaluated in further studies [152,153].

Myocardial perfusion

Myocardial perfusion imaging (MPI) has proven to be a valuable methodology for assessing the physiologic significance of a stenosis, allowing both a reliable diagnosis and prognosis in patients with CAD to be made [4,22,154–156]. Pharmacologic-induced coronary vasodilation during the infusion of radionuclide tracers has been shown to be as accurate as exercise stress testing with single-photon emission tomography in diagnosing coronary disease [22]. However, sensitivity and specificity of stress testing has been described to be limited with accuracies ranging from 70 to 86%, typically detecting CAD in later stages when significant coronary stenosis is present [157]. By contrast, the morphological evaluation of coronary arteries with CT coronary angiography and the limited ability for dynamic evaluations of the myocardial contrast medium passage with multislice CT have thus far been proven to be unsatisfactory to assess the physiological significance of coronary artery stenosis. Studies investigating the relationship between stenosis of 50% or more at CT coronary angiography and corresponding myocardial perfusion defects at nuclear imaging demonstrated a relatively weak correlation for detecting reversible myocardial perfusion defects with a sensitivity and specificity ranging between 85–95 and 53–79%, respectively [158–160]. Only increasing cut-off thresholds to degrees of stenosis of 70% or more prompted a significant increase in agreement between CT and nuclear studies [158,160]. On the other hand, a comprehensive assessment of myocardial perfusion from physiologic testing and morphologic evaluation of the coronary arteries by means of image fusion of nuclear imaging and coronary CT angiography has been shown to provide incremental diagnostic value over either technique alone. Nevertheless, obtaining diagnostic information on coronary artery morphology and the corresponding myocardial perfusion using one single modality remains a coveted goal [158–160].

Initial research efforts to perform CT myocardial perfusion imaging date back to the era of electron-beam CT and four-row

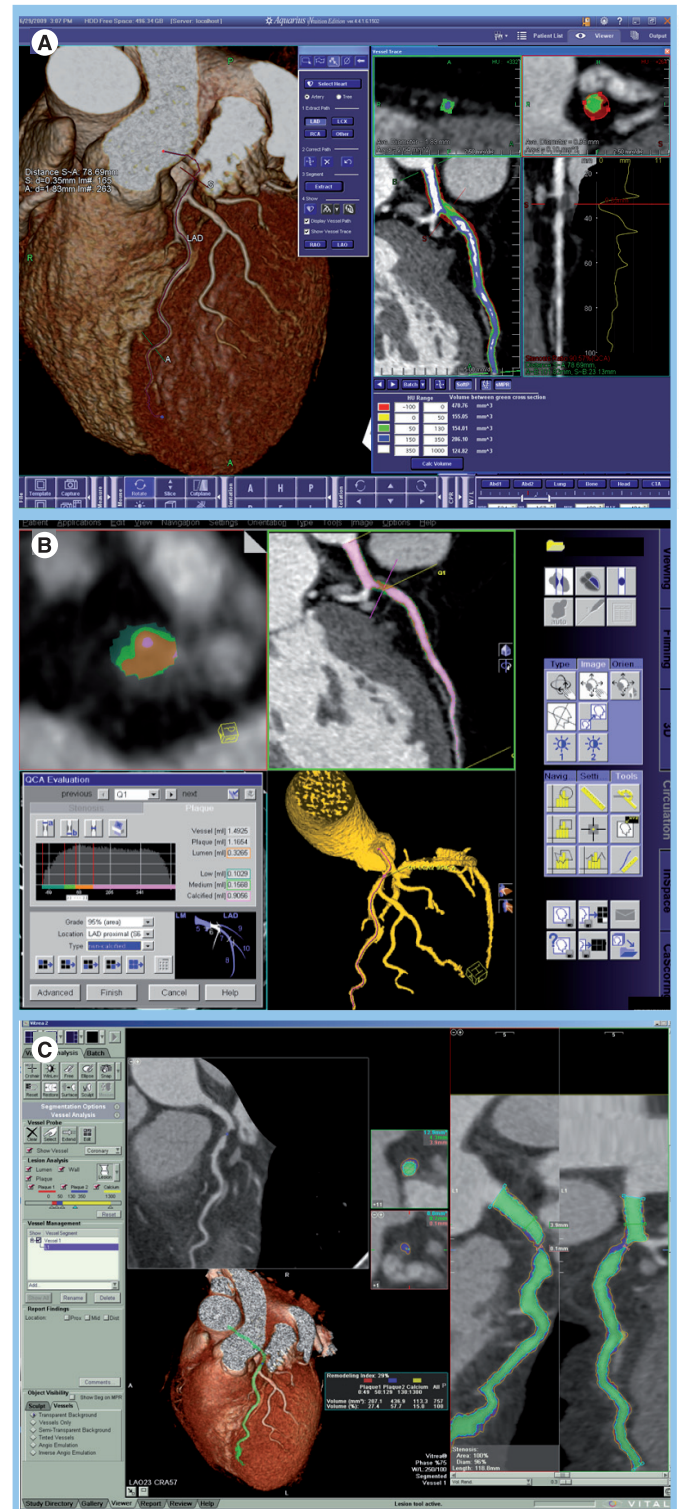


Figure 2. Overview of different commercially available software solutions allowing dedicated plaque analysis and characterization. (A) Circulation (Siemens Healthcare, Erlangen, Germany); (B) Aquarius (TeraRecon, CA, USA); (C) Vitrea (Vital Images, MN, USA).

MDCT, which revealed acute myocardial infarctions as hypo-attenuated myocardium in animal models [161,162]. The early

introduction of these observations into clinical practice showed 91% sensitivity, 79% specificity and 83% accuracy for the CT detection of myocardial infarction [163].

However, only the introduction of the most recent technological advances suggests the feasibility of CT as a standalone modality for an integrative evaluation of all aspects of coronary heart disease [46,47,164–168].

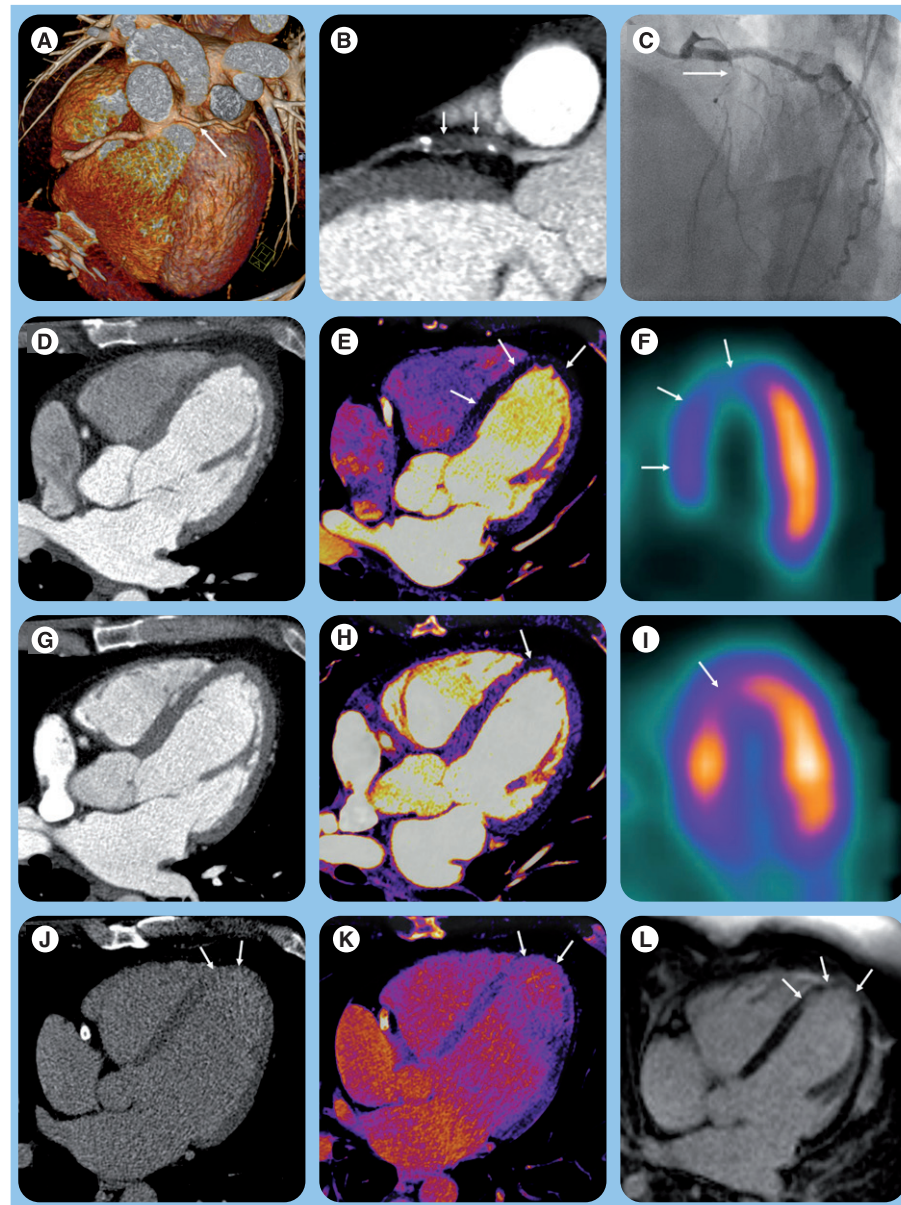


Figure 3. A 45-year-old man presenting with atypical chest pain. (A) Volume-rendering technique and **(B)** computed tomography (CT) coronary angiography illustrate a complete occlusion of the proximal left anterior descending artery (LAD; arrows), which was confirmed by **(C)** invasive coronary angiography. **(D)** While the merged gray scale image of myocardial stress-perfusion CT reveals no definite hypo-enhancement of the left ventricular myocardium, **(E)** the four chamber view of adenosine induced stress dual-energy CT (DECT) depicts an extensive perfusion defect (arrows) at ventricular septum and apical portion of the left ventricle, which is verified by **(F)** SPECT. **(G)** The merged grayscale image of rest perfusion CT study also shows normal myocardial contrast enhancement. However, rest **(H)** DECT and **(I)** SPECT demonstrate a partially reversible perfusion defect (arrows) in the corresponding LAD territory. **(J)** Delayed enhancement CT identifies subtle delayed hyper-enhancement (arrows) at the left ventricular apex of the left ventricle. The apical iodine uptake is visualized more prominently at the iodine map of **(K)** DECT and confirmed by **(L)** delayed-phase MRI (arrows).

In their study George *et al.* compared the combination of CT coronary angiography and rest–stress CT myocardial perfusion imaging to detect hemodynamically significant stenosis, with the combination of rest–stress single photon emission CT (SPECT) and quantitative coronary angiography as the reference standard using adenosine stress 64- and 256-row CT in 40 patients with abnormal myocardial perfusion SPECT findings [23]. They reported 86% (79%) sensitivity, 92% (91%) specificity, 92% (75%) positive-predictive value and 85% (92%) negative-predictive value on a per-patient (per-vessel territory) analysis, with an estimated mean effective radiation dose of 21.6 mSv for the combined rest and stress 256-row CT imaging and 16.8 mSv for the 64-row stress CT examinations. Initial studies applying DSCT in dual-energy mode have reported good correlation between CT and SPECT studies for detecting decreases in the myocardial blood supply [46,47]. Since dual-energy CT data can be postprocessed in different ways it may have the potential for the detection of obstructive CAD and simultaneously provide information about the hemodynamic consequences of detected lesions on myocardial perfusion from a single dual-energy CT acquisition. **FIGURE 3** provides an example of a perfusion study in a patient presenting with atypical chest pain.

Moreover, second-generation DSCT scanners might be capable of performing dynamic first-pass myocardial CT perfusion (**FIGURE 4**). According to initial studies, adenosine-stress dynamic volume CT myocardial perfusion can provide comparable results to MRI for the differentiation between normal and ischemic myocardium, and for the determination of semiquantitative parameters of myocardial blood flow with high specificity and a low rate of false-positive findings [169,170]. In addition, the results of these studies suggest the feasibility of dynamic first-pass perfusion CT to obtain absolute quantitative parameters

of myocardial blood flow as a moderate correlation between absolute myocardial blood flow quantification and the upslope of the signal intensity over time curve was observed.

Further research efforts are being directed towards optimizing the visualization of perfusion abnormalities. The results of a recent study suggest that minimum-intensity projection and thick multiplanar reformation might be beneficial in the qualitative and quantitative evaluation of infarcted myocardium [171].

Myocardial viability

The identification of dysfunctional but viable myocardium in patients with CAD is of paramount clinical importance since viable myocardium most likely benefits from revascularization, whereas revascularization of scar tissue will not lead to improvement of left ventricular function [172]. Myocardial viability has traditionally been assessed by using nuclear techniques [173,174]. However, the concept of delayed contrast enhancement has been successfully implemented with MRI to identify the location, extent and transmuralty of myocardial infarction [175,176]. MRI delayed enhancement imaging reliably detects myocardial scarring and is used clinically to detect occult infarcts, to predict functional recovery after revascularization therapy and to identify risk for future adverse cardiac events, making it the clinical reference standard [177–181].

Delayed enhanced imaging using MRI detects accumulations of gadolinium-based contrast material in areas of myocardial necrosis after infarction [175]. In theory, the same principle may apply to cardiac CT since iodine-based intravenous contrast has similar kinetics as gadolinium. It has been repeatedly shown in animal studies that CT can detect iodine accumulation in irreversibly damaged myocardium [182,183]. Furthermore, delayed-enhancement CT has been shown to correlate well with MRI during the different stages of infarction, enabling the assessment of reperfusion during acute, subacute and chronic stages, as well as the accurate degree of transmuralty [184–186]. In humans, delayed-enhancement CT and MRI also correlate well; however, CT systematically underestimates the true infarct size compared with MRI [187,188]. To date, no universal agreement on the most suitable protocol for delayed-enhancement CT imaging could be achieved as some studies indicate the highest difference in

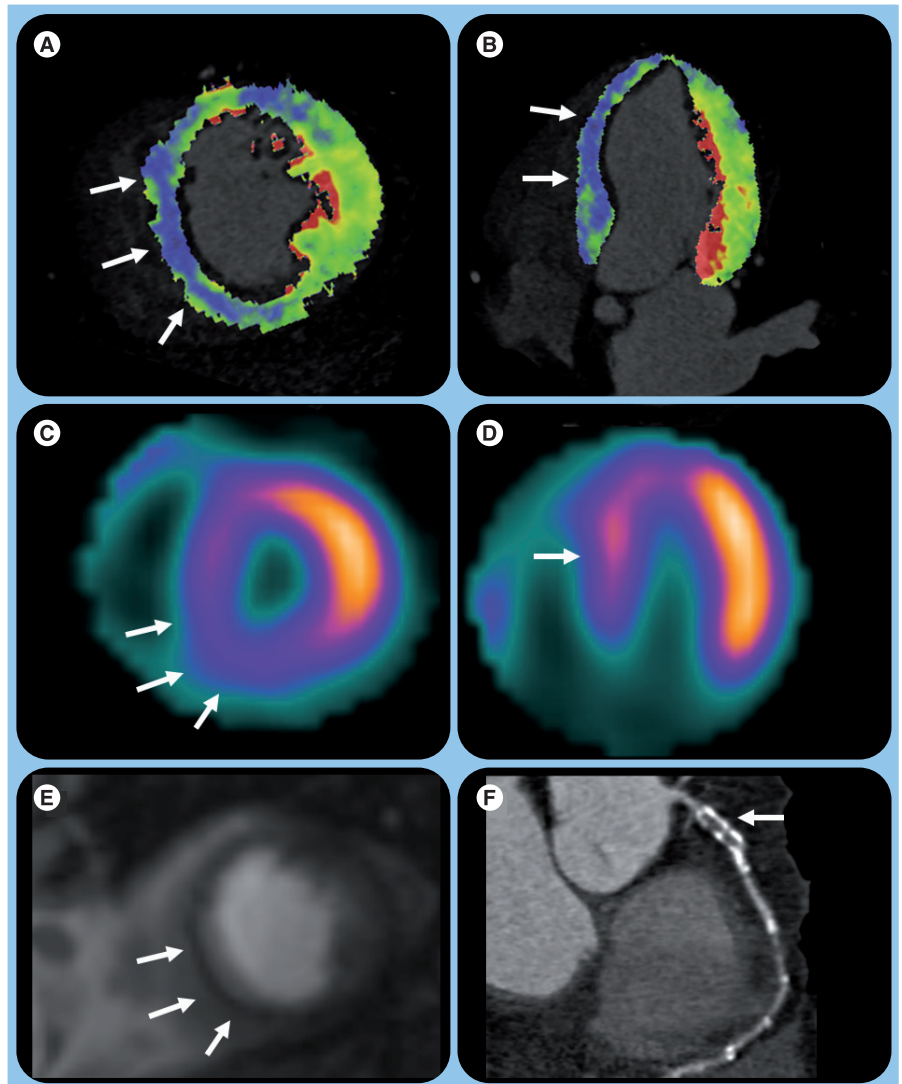


Figure 4. Dynamic real-time myocardial stress-perfusion in a 50-year-old man presenting with atypical chest pain using second-generation dual-source computed tomography. (A & B) The absolute quantification of the myocardial perfusion and resulting computed tomography (CT) myocardial blood pool perfusion maps reveal hypo-perfusion (blue color, labeled with arrows) most prominent inferoseptally in the mid-ventricular portion of the left ventricle with decreased myocardial blood flow of approximately 60 ml/100 ml/min. **(C & D)** CT findings were confirmed by SPECT and **(E)** stress-perfusion MRI. **(F)** Curved multiplanar reformat depicting a calcified and noncalcified plaque, causing occlusion of the proximal right coronary artery.

contrast attenuation between normal and infarcted myocardium occurred 5 min after intravenous contrast injection, whereas intervals of up to 15 min have been proposed by others as well as low-kilovoltage scanning protocols for better contrast differentiation [182,189].

The clinical value of CT viability imaging alone might be limited by the additional amount of radiation, which is approximately 3.8 mSv in female and 2.8 mSv in male patients [190]. However, the integration into a comprehensive scanning protocol might allow a non-invasive patient evaluation using a single modality and has the potential to provide safer and

cheaper assessment with less radiation than the current routine combination of nuclear myocardial perfusion imaging and conventional angiography.

Conclusion

Computed tomography has been recognized as the most valuable and potentially effective alternative to invasive coronary angiography for the detection and diagnosis of CAD. Owing to its rapid technological development, ongoing refinements and improved diagnostic accuracy, current technical limitations, including the association of coronary CT angiography with relatively high levels of radiation, are increasingly being addressed. The recent introduction of larger detector arrays and two generations of DSCT scanners brought substantial improvements in temporal resolution. New acquisition concepts such as 'high-pitch single-heartbeat acquisitions' have similar potential to reduce radiation dose. It can be expected that improved technology, ongoing development of scan protocols and appropriate clinical studies will further refine the role of cardiac CT in the near future, widening the scope of coronary CT angiography over mere anatomical assessment to a complete analysis of cardiac morphology, function, perfusion and viability. Currently, clinical applications seem most likely in the context of stable and acute chest pain to rule out coronary disease in selected subgroups of individuals who do not have a high pretest likelihood of disease and in whom a negative CT scan would replace an otherwise necessary invasive coronary angiogram.

With appropriate patient selection, it can be expected that cardiac CT can not only accurately diagnose all aspects of heart disease, but also markedly decrease healthcare costs and reliably predict clinical outcomes.

Expert commentary & five-year view

Computed tomography of the coronary arteries has been performed for more than three decades for the detection of coronary artery calcifications. Moreover, for the last 8 years contrast-enhanced CT coronary angiography has become a clinically accepted methodology for a non-invasive assessment of the coronary arteries achieving an angiographic display. In addition, with rapid innovations and ongoing refinements in technology, current technical limitations, including the association of cardiac CT with relatively high levels of radiation, are being increasingly addressed. Along with an increasing clinical evidence base, the healthcare community is working on appropriateness criteria and defining indication guidelines to guarantee suitable use, curb overutilization and ensure cost-effectiveness. New scanner technologies and innovative applications are constantly being explored and sustain a constant widening of the scope of cardiac CT over mere coronary artery assessment to the complete analysis of cardiac morphology, function, perfusion and viability. Considering all of the above, there is little doubt about the rapidly expanding role and growing importance of cardiac CT as a cornerstone for a comprehensive evaluation of all aspects of CAD.

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Key issues

- To date, the clinically accepted diagnostic value of computed tomography (CT) coronary angiography is focused on a mere morphological evaluation.
- Currently, there is no single modality available to comprehensively evaluate all aspects of coronary artery disease including morphology, function, perfusion and viability.
- Current limitations of cardiac CT include limited temporal resolution, especially in patients with high resting heart rates and irregular heart rhythm, and high levels of radiation exposure.
- Ongoing innovations in scanner technology and acquisition protocols continue to improve the performance and clinical scope of cardiac CT, and enable substantial reductions in radiation exposure.
- Technologies and acquisition protocols are currently being investigated to combine coronary CT angiography with CT-based methods for the evaluation of myocardial function, perfusion and viability to allow a comprehensive assessment of all aspects of coronary artery disease with CT as the sole imaging modality.

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