Making movies of the brain's electrical potentials: NICER Neuroscience of Magination & A A practical procedure for dynamic source localization analysis with validating simulation



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INTRODUCTION

- Event-related potentials (ERPs) average time-locked data taken from multiple electroencephalogram (EEG) trials, thereby allowing analysis of a specific electrophysiology process within a certain time window. [1]
- Despite their high temporal resolution, ERPs offer poor spatial resolution which leads to difficulties in localizing latent neural generators, an issue commonly known as the "inverse problem." [2]
- Dipole source localization analysis (DSLA) yields solutions for the inverse problem and can supplement ERP findings with anatomical details. [3] DSLA may result in underqualified data when studying a large area of the brain, or with an unpredictable number of active regions occurring at different times. [4,5]

RESULTS

- Regression analysis between the actual child data (Fig.A) and the dynamically-guided DSLA simulation data (Fig.B) showed high fit, $R^2 > 0.97$ (p < 0.005), with the exception of the data at 695ms ($R^2 = 0.40$; p = 0.47).
- Comparison with the "static" DSLA simulated adult data (Fig.C) revealed that dynamicallyguided DSLA modelling and simulation produced a higher fit with the actual child data. This comparison shows large differences in the timing attributed by ACT-R to the same sources

OBJECTIVES

- Determine a practical procedure which may permit to narrow down DSLA within the most relevant time windows and test their validity through simulation.
- Use this novel procedure, called *dynamically-guided dipole source localization analysis*, to appropriate pre-existing tools for the purpose of accurately examining and analyzing the neurofunction of distinct demographic groups despite limited MRI data and normalized templates.

MATERIALS AND METHODS

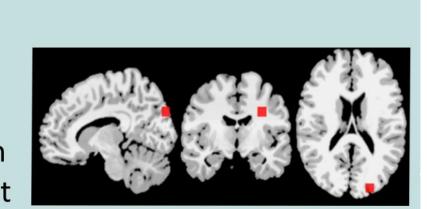
Step 1 – ERPs from EEGs:

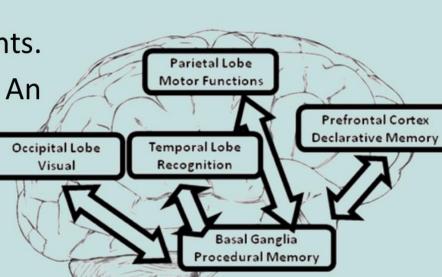
Reprocessed ERP data collected from preschool -Ac ---children (n=26, mean age=4.12) performing a visual sustained attention task with target and distractor stimuli.

ICA-2

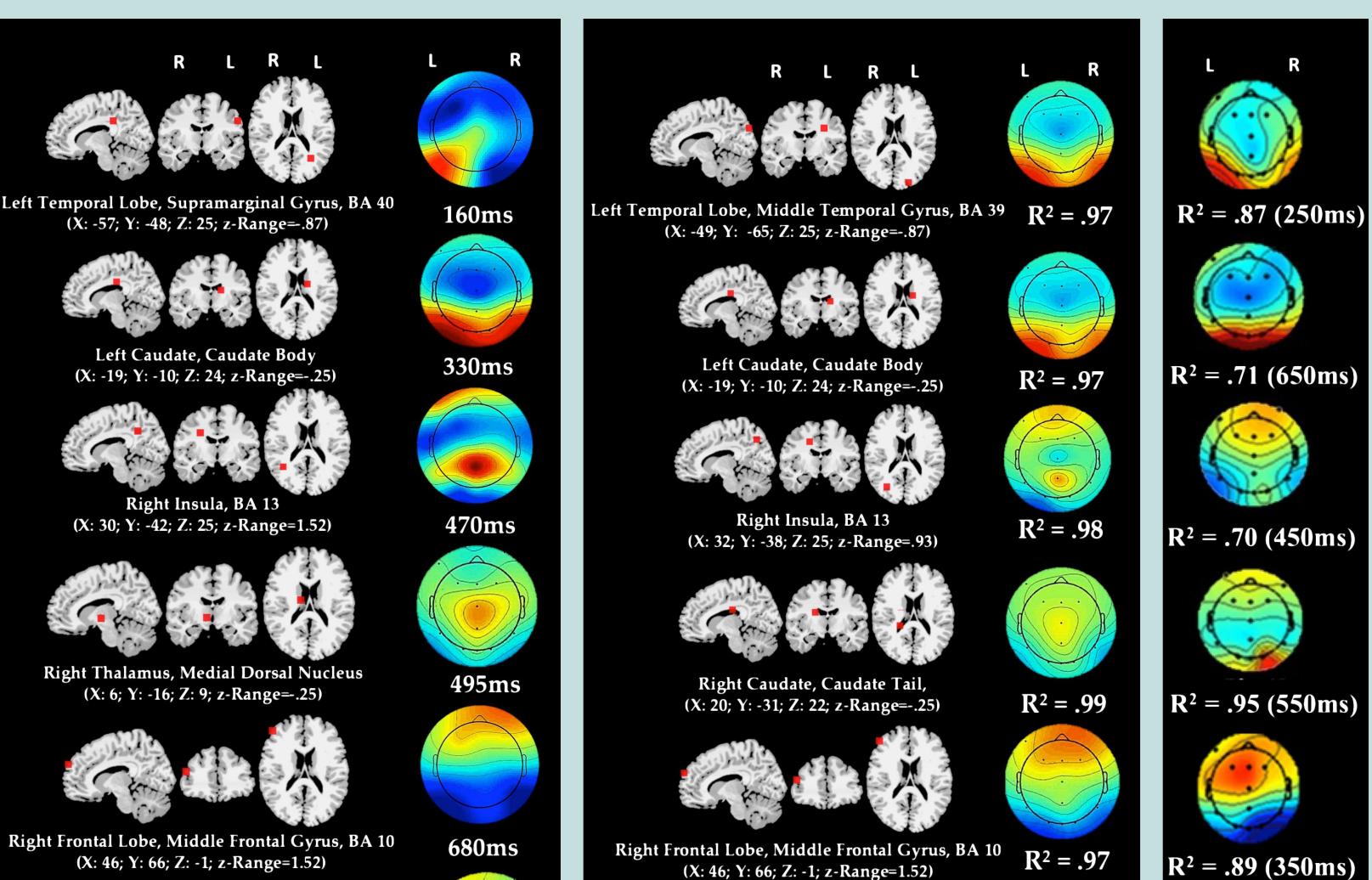
ICA-4

Step 6 – Dipole Analysis, Talairach Labelling: The **DIPFIT** component of EEGLAB was used to estimate a set of dipoles in the averaged ERP data that would explain the independent components. Step 2 – Independent ICA-8 Step 7 – ACT-R Model: An adapted version of Adaptive Control of Visual Thought-Rational was used to model and simulate data.





under the two DSLA approaches, indicating important deviation from homology in the putative sequence of neural processes.









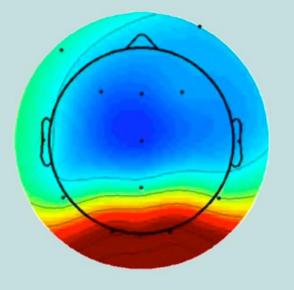
Components Analysis: ERP components were identified using the EEGLAB FASTICA algorithm.

Step 3 – Identify Max ERP Activity Path: Differences in ERP waveforms between target and distractor conditions were interpreted via ERP activity path analysis.

Step 4 – Topographical Maps, Movie Review & Snipping: Topographic maps were created to represent epochs of averaged ERPs and assembled as movie clips.

Step 5 – Topographical Maps, Standstill: Maps were selected for further analysis.

Latency 85 ms from DT Expl



Step 8 – Simulated ACT-Rbased Spike-series: Simulated electrical activity in the brain using the neurocognitive model. Calculated the resulting electric field at the surface of the head for each electrode.

Step 9 – Simulation of ERP Topographical Maps, Standstills: Simulated electrical activity in the brain using the neurocognitive model and calculated the resulting voltage at each electrode. Simulated maps were created by converting the ACT-R spike-series into a relative voltage scale (with range from blue/black, -6µV, to red/orange, 6μV). Latency 85 ms from DT Sim

Final Step – Validation Test: Compare the ERP activity of real and simulated sources.



Right Parietal Lobe, Precuneus, BA 7 (X: 5; Y: -69; Z: 54; z-Range=-.25)

Fig.A: Actual child data

695ms

Right Occipital Lobe, Cuneus, BA 18 (X: 19; Y: -85; Z: 23; z-Range= -1.44)

 $R^2 = .40$ $R^2 = .95 (150ms)$

Fig.B: Dynamically-guided DSLA simulation data

Fig.C: "Static" DSLA adult simulation data

CONCLUSIONS

- These findings demonstrate that readily available modeling and simulation tools can be appropriated to reliably fit the neural responses and corresponding behaviours of an understudied demographic sample.
- It may be possible to employ dynamically-guided DSLA as a method to identify structural and functional similarities within and between populations, this could have a variety of applications across multiple disciplines, which include: examining specific characteristic biomarkers of neurodevelopmental disorders, informing and evaluating the effectiveness of specific interventions, investigating the efficacy of educational strategies, and more.
- The specific components employed by this iteration of dynamically-guided DSLA can be replaced by more powerful and accurate techniques as they become available, while the analytical framework and objective of producing comparable visualizations of neural activity in a studied demographic and a simulation model remain unchanged.
- The modular nature of dynamically-guided DSLA is what makes it a particularly suitable technique in a field of study where rapid technological progress is the expected norm, and it affords many opportunities for future research and development into its application as a valuable process of examining neurofunction.



REFERENCES

1. Rugg, M., & Coles, M. (1995). Electrophysiology of mind event-related brain potentials and cognition. Oxford University Press.

2. Sanei, S.; Chambers, J.A. EEG Signal Processing; 1st ed.; Wiley-Interscience: Chichester, West Sussex, UK, 2007.

3. Bathelt, J.; O'Reilly, H.; de Haan, M. Cortical Source Analysis of High-Density EEG Recordings in Children. J. Vis. Exp. 2014, e51705, doi:10.3791/51705.

4. Darvas, F., Pantazis, D., Kucukaltun-Yildirim, E., & Leahy, R. (2004). Mapping human brain function. Neuroimage, 23, S289–S299. https://doi.org/10.1016/j.neuroimage.2004.07.014

5. Hämäläinen, M., & Ilmoniemi, R. (1994). Interpreting magnetic fields of the brain: minimum norm estimates. Medical & Biological Engineering & Computing, 32(1), 35–42. https://doi.org/10.1007/BF02512476

