



Continuous Manufacturing and Molecular Modeling of Pharmaceutical Amorphous Solid Dispersions

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Abstract

Amorphous solid dispersions enhance solubility and oral bioavailability of poorly water-soluble drugs. The escalating number of drugs with poor aqueous solubility, poor dissolution, and poor oral bioavailability is an unresolved problem that requires adequate interventions. This review article highlights recent solubility and bioavailability enhancement advances using amorphous solid dispersions (ASDs). The review also highlights the mechanism of enhanced dissolution and the challenges faced by ASD-based products, such as stability and scale-up. The role of process analytical technology (PAT) supporting continuous manufacturing is highlighted. Accurately predicting interactions between the drug and polymeric carrier requires long experimental screening methods, and this is a space where computational tools hold significant potential. Recent advancements in data science, computational tools, and easy access to high-end computation power are set to accelerate ASD-based research. Hence, particular emphasis has been given to molecular modeling techniques that can address some of the unsolved questions related to ASDs. With the advancement in PAT tools and artificial intelligence, there is an increasing interest in the continuous manufacturing of pharmaceuticals. ASDs are a suitable option for continuous manufacturing, as production of a drug product from an ASD by direct compression is a reality, where the addition of multiple excipients is easy to avoid. Significant attention is necessary for ongoing clinical studies based on ASDs, which is paving the way for the approval of many new ASDs and their introduction into the market.

Keywords amorphous solid dispersions · bioavailability · continuous manufacturing · dissolution · melt extrusion · molecular modeling · solubility · spray drying

Introduction

One of the most significant hurdles in bringing a new drug candidate to the market is poor aqueous solubility, consequent low dissolution rate, and poor oral bioavailability. This has become more pronounced with the arrival of combinatorial tools and high-throughput technologies for screening for

the medicine discovery phase (1). The proportion of molecules that face this challenge, most commonly belonging to BCS class II and IV, is rising with each passing year (2–4). Low dissolution rate and poor bioavailability have an impact on the marketability of these drugs, with limited formulation strategies available to address the challenges (5), especially for BCS class II drugs, which display dissolution-limited absorption (6).

For a drug to be absorbed *via* the gastrointestinal epithelium, the dosage form first disintegrates, and the drug dissolves in the gastrointestinal fluids. To make this possible, newer formulation strategies need to be applied to enhance dissolution rate and solubility (1). There are multiple approaches that can be employed to achieve these goals, including prodrug formation (7), complexation (8), micronization (9), salt formation (10), micelles (11), nanoemulsions (12), solid–lipid nanoparticles (13), and nanocrystals (14).

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One strategy is to employ supersaturation-based formulations (15). A supersaturated solution is formed when the total solute concentration surpasses the equilibrium solubility. The augmented concentrations attained through the formation of a supersaturated solution consequently enhance the oral bioavailability of the molecule. A key drawback of a supersaturated solution is its metastability and the intrinsic inclination for the drug candidate to crystallize; thus, the solubility advantage is lost. One of the supersaturating formulation strategies, the amorphous solid dispersion (ASD), comprises a mixture of both amorphous drug and polymer at the molecular level, with increasing oral bioavailability in comparison to crystalline systems (16–19).

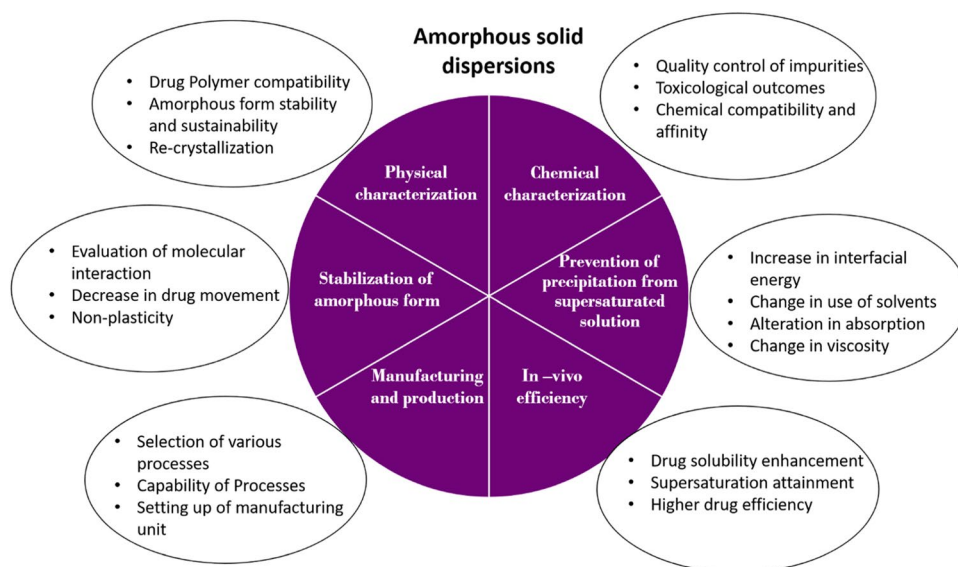
Although the precise factors that improve the dissolution of drug molecules from an ASD that lead to the formation of supersaturated solutions are not yet fully deciphered (Fig. 1), it has already been identified that the polymer employed in the formation of the ASD plays an essential role in facilitating drug release from the ASD and in delaying consequent crystallization (20). This is especially significant for drugs that crystallize rapidly because once crystallization begins, solubility enhancement is compromised as the supersaturation level goes down. Therefore, the polymer employed in an ASD should possess both hydrophobic and hydrophilic moieties to prevent crystallization of the drug in the aqueous environment while also facilitating drug release from the ASD (21–23).

Although the concept of ASDs has created immense interest within the scientific community, this has not been translated into the desired commercial success. ASD-based formulations that have reached the market remain in double digits. This low number originates from problems with scale-up and instability of the ASD during the manufacturing process (24, 25). The experimental screening of different

candidates as polymeric carriers while developing an ASD system is a slow, tedious, and costly process. Another difficulty lies in ensuring long-term product physical stability, as drug recrystallization from its initial amorphous state and phase separation between the drug and polymeric carrier can cause unacceptable variations in oral bioavailability (26). Even though ASDs came into existence more than half a century ago, the concepts of formation and physical stability of ASDs are still not fully understood. Accurately predicting interactions between the drug and polymeric carrier requires long experimental screening methods. As a result, product development is attained through trial-and-error methods that end up increasing cost and stretching timelines (27). The time can be lessened by acquiring suitable knowledge about the behavior of ASD formation, dissolution, and subsequently drug release from the carrier matrix. This is where molecular modeling tools come into the picture. Computational tools hold the potential to act as a novel paradigm in the research and development of ASDs.

Technologies that may be employed to manufacture ASDs include hot melt extrusion (HME), KinetiSol®, spray drying, supercritical fluid (SCF) technology, and electrospinning (28). HME is an organic solvent-free continuous operation in which a physical mixture of active pharmaceutical ingredient (API) and polymeric carrier is melted, extruded, and solidified, with varying processing parameters which include feed rate, temperature, shear force, die size, geometry, screw type, and speed (29, 30). KinetiSol® is a novel high shear-based technology that also employs the fusion principle wherein shear force and friction rapidly transform the physical mixture into the melted state to give a homogeneous ASD (19). Spray drying is another technology commonly employed in the production of ASD systems. Spray drying is a fast-drying process that causes kinetic

Fig. 1 Overview of key factors when developing amorphous solid dispersions



entrapment of the API in the amorphous state. Spray drying conditions, such as solvent content, can have a significant influence on spray-dried dispersion characteristics (31). It has been proven that supercritical fluid technology maintains polymeric structure more than any other methodology, and it is a one-step process. It may be utilized at low temperatures, enabling thermolabile drugs to be processed without surpassing the glass transition temperature (T_g). The residual solvent content in processed samples is kept to a bare minimum (32). Electrospinning (ES) is a unique technique for making ASDs out of a polymer mixture or melt. Using ES, micro- and nanometric polymer fibers are created by the generation and elongation of an electrified fluid element. ES, in contrast to the abovementioned ASD-producing techniques, functions at ambient temperatures, making it a mild process at a low cost. The API is distributed in a polymer matrix at the molecular level, resulting in a nano-scale amorphous solid dispersion in electrospun fibers with a large surface area (33).

Continuous manufacturing refers to the production of a pharmaceutical product in a single continuous process. The entire process takes place in one location, from beginning to end, with no waiting times. Continuous manufacturing is a more flexible method than batch processing that allows for better production scaling. Generally, high-volume goods drive the adoption of continuous processing, which is the motivation for using continuous processes mostly in the commodity chemical industry. While high capacity is still an important aspect of continuous manufacturing, reducing development costs for novel drugs and increasing flexibility to create capabilities of tailored therapeutics for specific patient populations are other factors for the shift from batch to continuous manufacturing (34). Continuous manufacturing offers high-quality products as the whole process may be controlled using process analytical technology (PAT).

This review addresses new advances in the field of ASDs that aim to overcome the issues that limit the marketability of such formulations and considers new approaches that can enable the formulation of ASDs with more confidence. Special emphasis has been given to molecular modeling techniques that can be used to address some of the burning questions related to ASDs today. It also throws new light upon the continuous manufacturing techniques that can overcome the challenge of scale-up for ASDs.

Amorphous Solid Dispersions and Mechanism of Enhanced Dissolution

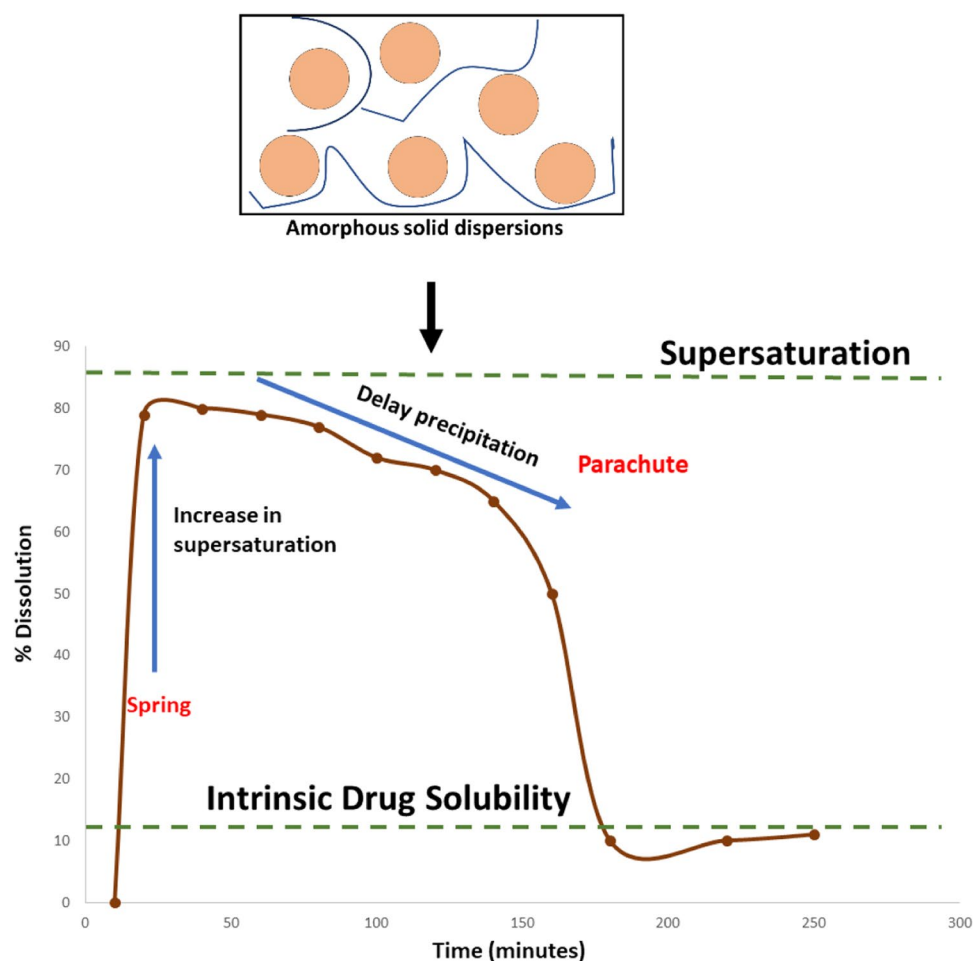
Amorphous materials exist in a thermodynamically metastable state, and because of the significantly higher free energy compared to crystalline solids, amorphous forms are more soluble (35). Amorphous materials may exist as supercooled

liquids that can be achieved by fast cooling of a melt. As the material is further cooled, the molecular mobility is gradually reduced, and the viscosity increases simultaneously. The temperature at which this transition happens is called the glass transition temperature (T_g), and below the T_g the material is called “glassy” (35, 36). The T_g is related to alterations in a number of thermodynamic parameters, including enthalpy, entropy, and volume (36).

ASDs represent a promising formulation strategy to increase the aqueous solubility and dissolution rate and oral bioavailability of poorly water-soluble drugs (37). In an ASD, the API, which is initially crystalline and hydrophobic, is made to disperse in a carrier matrix that is hydrophilic in nature. This strategy offers advantages of amorphization associated with decreased particle size and enhanced wettability (38). For example, Harmon *et al.* performed research on the mechanism of dissolution-induced nanoparticle formation from a copovidone-based solid dispersion. The surfactant inside the ASD particle inhibited “hydrophobic capture,” a process that resulted in fast, local drug domain aggregation. This inhibition enabled amorphous drug domains to diffuse into the bulk solution where they were characterized as nanoparticles (42). Similarly, Han F *et al.* investigated the impact of phase separation morphology on the mechanism of drug release from ASDs and found that release at low drug loadings was influenced by erosion of the polymer and embedded drug-rich droplets (39), while at high drug loadings, the creation of a drug-rich domain continuous morphology resulted in the preferential release of polymer-rich domains (43).

ASDs hold the potential to address bioavailability issues as the drug molecule exists in its amorphous form, which is known to have higher solubility. This solubility enhancement, along with higher rates of dissolution and improved solid-state stability, can be accomplished by the selection of a suitable polymeric carrier. The spring and parachute concept was explained, where a higher spring effect (dissolution) and enhanced parachute effect (crystallization inhibition) were observed (40). The “spring and parachute” mechanism of enhanced dissolution by amorphous solid dispersions is depicted in Fig. 2, with the polymer providing the parachute, which maintains the supersaturation of the drug. “Spring” is a descriptive word for the initial drug dissolution. After supersaturation is achieved, liquid-liquid phase separation or drug crystallization can cause drug concentration to decrease, and interaction of drug and polymer is required in order to provide a “parachute” and maintenance of drug supersaturation (41). The spring and parachute must be thoroughly adjusted so that an appropriate degree of drug supersaturation can be achieved (an optimal spring) and sustained over time (an effective parachute) (42). The polymeric carrier also plays a vital role in stabilizing the ASD system in the solid state also, by decreasing the molecular mobility

Fig. 2 Spring and parachute mechanism of enhanced dissolution by amorphous solid dispersions



and increasing its T_g , maintaining the drug in the amorphous state. The stability of such a system is influenced by the drug-polymeric carrier interactions and intermolecular interactions in the drug's crystal lattice.

Absorption of drugs from ASD is a multistep process that has three stages. In the first step, the ASD undergoes dissolution in the surrounding medium, followed by the uptake across the intestinal membrane of the solubilized drug from the medium, with the final step causing the drug to attain equilibrium of drug in the drug solution (43). During dissolution, the ASD system exists in a state of metastable equilibrium such that, due to the lack of any crystalline substance, a transition state between the drug's amorphous phase and its solution form exists. Drug-rich particles are said to be naturally metastable in an amorphous liquid phase transition. The amorphization contributes to a better dissolution as amorphous compounds possess higher energies and apparent solubilities as compared to their crystalline counterparts. This is due to their disordered structure and higher energetic state, which does not have the prerequisite of breaking down the crystal lattice before dissolution (44). A crucial step in the enhanced dissolution profile of the drug

is the formation of dissolved ASD, as it is directly associated with oral bioavailability. Two possible mechanisms of drug release from an ASD are (a) carrier-controlled release and (b) drug-controlled release, which have been proposed to explain the mechanism of dissolution of ASD (45, 46). The diagrammatic representation of the overall enhancement of aqueous solubility and oral bioavailability by ASDs is depicted in Fig. 3.

Carrier-Controlled Release

In carrier-controlled release, polymer employed does not dissolve, and after ingestion of dissolution medium, they form a viscous gel like structure. This viscous gel layer structure shows two layers; one is diffusion layer (between dissolved and undissolved API), and another is erosion layer (between viscous gel and dissolution medium) (47). Erosion and release of drug from these layers depends on the nature and interaction of drugs and polymers (48). There are multiple reports where carrier-controlled release is found congruent. Indulkar *et al.* studied that hydrophilic polymer shows carrier-controlled release at low drug loading (22).

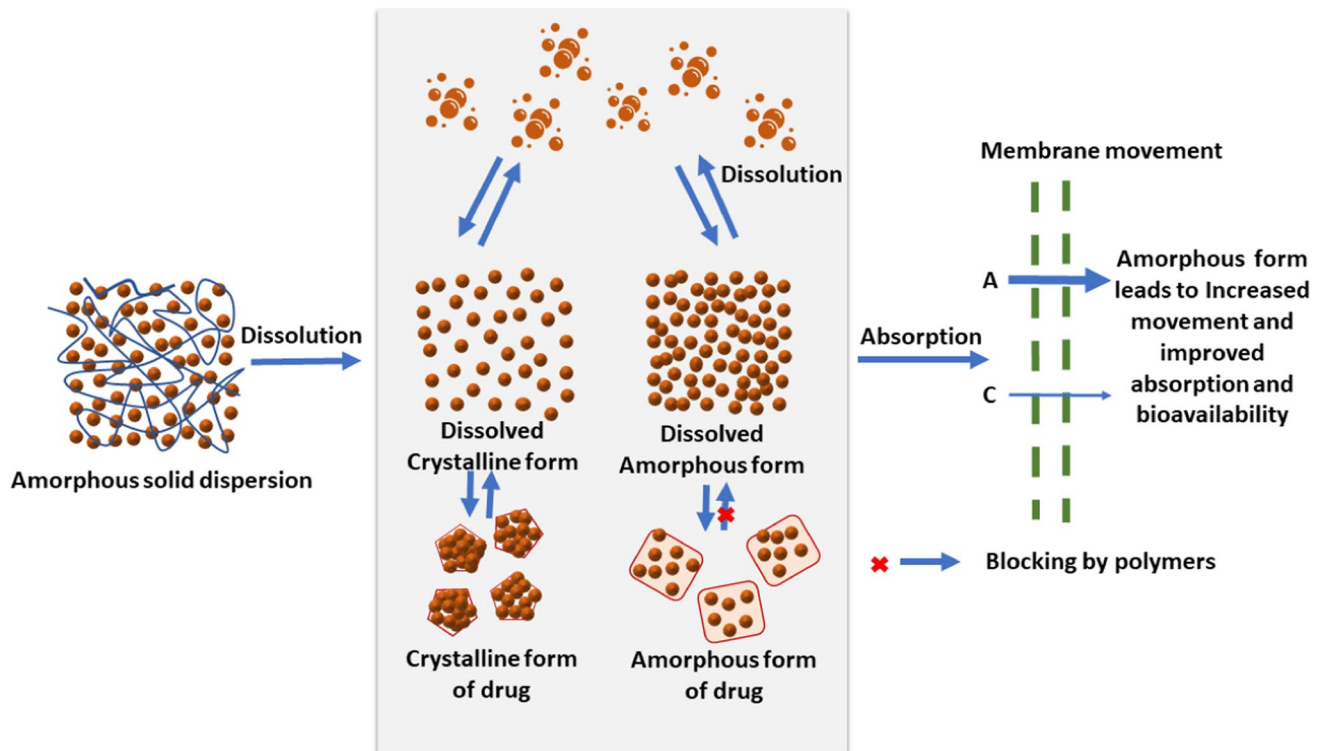


Fig. 3 Schematic presentation of overall enhancement of solubility and bioavailability by amorphous solid dispersions

Saboo *et al.* observed the formation of nano-droplets through the amorphous liquid phase separation (ALPS). Nanodroplets are drug-rich aggregates which forms when the drug amorphous solubility is exceeded and ALPS happens (49). It has been observed that some ASDs with a low drug loading dissolve to a concentration higher than the amorphous solubility of the drug which leads to ALPS. This ALPS further cause generation of drug-rich amorphous aggregates of nanometer size. These aggregates are colloidal in nature, and they coexist with the aqueous phase. The aqueous phase already contains drug concentration equivalent to the amorphous solubility. Once the dissolved drug absorbs, these aggregates release drug in to the medium and maintains the amorphous solubility and membrane flux (47).

Drug-Controlled Release

In drug-controlled release, the employed polymer dissolved completely, and due to which no viscous gel layer formation happens (46). As the polymer and drug dissolves at different rates (noncongruent), super-saturation happens at fast pace which further increases the chances for crystallization. Amorphous drug-rich aggregate (nano-droplet) formation does not happen in this scenario as amorphous drug state is not stable. Indulkar *et al.* and Saboo *et al.* observed that

hydrophilic polymer shows drug-controlled release at high drug loading (22, 48, 49).

Amorphous Solid Dispersion Development.

ASDs represent a formulation approach that has been extensively used to improve drug solubility, enhance oral bioavailability, and mask taste. One or more active pharmaceutical ingredients (APIs) are distributed in a nonreactive polymer or matrix (50). It is recognized that molecular level mixing with a polymer of hydrophilic nature improves the release of poorly water-soluble chemicals from ASDs. The polymer type and drug loading in the ASD have been proven to affect the release rate. Rapid release of ASD components happens in some cases, often with minimal drug loading, resulting in apparent solution concentrations greater than the amorphous solubility of the drug (51). Figure 1 describes the factors affecting the development of ASDs. Cho and co-workers 3D-printed orodispersible films loaded with amorphous olanzapine (52). Tres *et al.* generated amorphous materials from supersaturated aqueous solutions of ritonavir and lopinavir by antisolvent addition and showed that the dissolution of both the drugs was improved when made into ASDs compared to the crystalline form (53). Feng *et al.*

focused on using an ASD-based polymer-surfactant system to improve the aqueous solubility and oral bioavailability of itraconazole and efavirenz (54). Kwon *et al.* used a spray drying process, where a hydrophilic polymer was successfully employed to incorporate the hydrophobic drug atorvastatin, into solid dispersions. Atorvastatin in the ASD form resulted in higher solubility and an improved dissolution profile compared to the crystalline drug (55). Solid dispersions of dolutegravir prepared by quench cooling and solvent evaporation methods showed increased bioavailability over its crystalline equivalent (56). Posaconazole kinetic solubility was improved by ASDs prepared by solvent evaporation, which resulted in an improved dissolution and bioavailability compared to the crystalline free drug (57). Figueirêdo *et al.* employed the ASD approach to combine two synergistic antichagasic drugs, posaconazole, and benznidazole, in the amorphous form demonstrating improved solubility and potentially enhanced bioavailability (58). In one study, it was found that using HME technology to prepare ASDs of lacidipine with Soluplus and PVP VA64 improved the drug's solubility and bioavailability (59). ASDs prepared using the KinetiSol technology improved abiraterone's solubility and pharmacokinetics (60). Ketoconazole was converted into an amorphous state with drug-polymer interactions, which yielded positive results (61). The researchers prepared PVAs with varying levels of cross-linking and hydrolysis, which were then evaluated in their solid dispersion formulations with amenamevir and looked into the differences in solubility improvement produced by different degrees of hydrolysis and degrees of polymerization (62). Candesartan and cilexetil ASDs were successfully developed using a ball milling approach (63). Quercetin ASDs were prepared using HME, which resulted in an increased dissolution rate and oral bioavailability. Similarly, celecoxib ASDs prepared by hot melt extrusion showed an improved dissolution rate (64). Ibuprofen ASDs generated using supercritical fluid technology showed improved absorption and oral bioavailability (65). Alhayali *et al.* investigated the ASD formulations of ezetimibe and the supersaturation-precipitation-permeation interactions and bioavailability increase of the API (66). The wettability improvement and bioavailability enhancement proved the success of the ASD approach in improving griseofulvin (GF) release from a ternary GF-Soluplus-SDS ASD (67). Solvent evaporation was used to create lacidipine-spirolactone co-amorphous solid dispersion (LCDP-SPLC ASDs) systems. *In vitro* release characteristics and physical stability were improved in the LCDP-SPLC ASDs systems compared to free drugs (68). These studies demonstrate that ASDs is a promising technique to fine-tune the release of drugs that are poorly soluble.

Due to the unique benefits and qualities of ASDs, the pharmaceutical industry has become extremely interested in methods for their manufacture. For instance, academics

have been interested in HME, an environmentally friendly technique, because of its capacity for continuous manufacturing. However, the industry also recognizes the value of spray drying for manufacturing solid dispersions which cannot be handled by HME. HME is not suitable for heat sensitive drugs and polymers with higher heat processing temperatures, a drawback that can often be resolved by using plasticizers. The KinetiSol® dispersion technology is a revolutionary alternative thermal processing method that relies on the combinatorial principle of shear force and friction to quickly turn the physical mixture into a molten state and create a homogenous ASD. The physicochemical characteristics of the drug and the polymers required to produce a thermally and chemically stable product must be considered when choosing an effective technique for manufacturing ASDs. Himawan *et al.* formulated ASDs of BCS class II drug valsartan by solvent evaporation to increase its oral bioavailability (69). Muller *et al.* formulated regorafenib amorphous solid dispersions to increase the biopharmaceutical performance (70). Similarly lumafentrine (71), filgotinib (72), atorvastatin (73), celecoxib (74), berberine (75), and tacrolimus (76) ASDs were prepared using solvent evaporation to enhance their biopharmaceutical properties. Nieto *et al.* prepared ASDs by a solvent casting method for solubility enhancement of fenretinide (77). Ewings *et al.* prepared ASDs of indomethacin using HME to increase the solubility (78). Sarode *et al.* enhanced the aqueous dissolution and biphasic partitioning by preparing ASDs of felodipine (79). Jijun *et al.* prepared nimodipine ASDs by HME with polyvinylpyrrolidone/vinyl acetate copolymer to increase the dissolution (80). Hassouna *et al.* prepared ASDs of ibuprofen by an emulsification-diffusion method to enhance its biopharmaceutical properties (81). Similarly ascorbic acid ASDs was prepared by Christina and co-workers (82). Paclitaxel ASDs were also prepared by freeze drying (83). Thombre *et al.* prepared ASDs of ziprasidone to enhance its solubility (84). Kim *et al.* increased the bioavailability of clopidogrel by preparing ASDs (85). In the same way sibutramine, ASDs were prepared by spray drying to enhance its biopharmaceutical properties (86). Deng *et al.* prepared ferulic acid ASDs by electrospinning (87). Mehanna *et al.* prepared ASDs of tadalafil by a fusion method for dissolution enhancement (88). Similarly, many more APIs were made into ASDs by different technologies as reported in Table 1.

Trend of Continuous Manufacturing of Pharmaceuticals

Over the last two decades, there has been a steep rise in the reports in the scientific literature on continuous manufacturing (Fig. 4).

When applying the term “continuous manufacturing” to “pharmaceuticals,” a similar trend with respect to the

Table 1 Literature Trend of Amorphous Solid Dispersions

Sr. No.	API	Polymers	Percentage of drug: excipient	Preparation method	Increase in solubility relative to pure API	Year	Reference
1.	Valsartan	Poly (vinyl pyrrolidone) K-30, poly (ethylene glycol) 6000, sodium alginate, calcium chloride, sodium dihydrogen phosphate, sodium bicarbonate	1:3	Solvent evaporation	60%	2022	(1)
2.	Regorafenib	Kollidon K25® (PVP), Affinisol 716G, 912G, and 126G (HPM-CAS), hypromellose, (HPMC)	17:3	Solvent evaporation	42%	2021	(2)
3.	Lumefantrine	Microcrystalline cellulose (MCC), Prodan, cellulose acetate phthalate (CAP), and pyrene	4:6	Solvent evaporation	33%	2020	(3)
4.	Filgotinib	HPMC (Methocel E5) HPMCAS (AS-MF grade), PVP K30	1:5	Solvent evaporation	13%	2018	(4)
5.	Atorvastatin	P188	1:5	Solvent evaporation	40%	2018	(5)
6.	Celecoxib	PVP (K29/32), PVP (K12), and PVP-vinyl acetate (PVP/VA) (Kollidon VA64). HPMCAS and HPMC	3:7	Solvent evaporation	45%	2017	(6)
7.	Berberine	Hydrogenated phosphatidylcholine	1:3	Solvent evaporation	60%	2015	(1)
8.	Tacrolimus	HPMC, croscarmellose sodium	1:49	Solvent evaporation	10%	2014	(7)
9.	Tranilast	HPMC, Kollidon VA64, and polyvinylpyrrolidone	1:9	Solvent evaporation	50%	2012	(8)
10.	Lansoprazole	Polyvinylpyrrolidone	1:3	Solvent evaporation	80%	2011	(9)
11.	Carvedilol	Porous SiO ₂ , Sylvania 350	1:50	Solvent Evaporation	50%	2011	(10)
12.	Risperidone	FlowLac® 100, Kollidon® CL-SF, magnesium stearate, Ac-Di-Sol, Avicel PH 102, methyl-cyclodextrin, and sodium starch glycolate	1:5	Solvent Evaporation	38%	2010	(11)
13.	Fenretinide	Polyvinylpyrrolidone K30 and triethyl-o-acetyl-citrate	1:9	Solvent casting	80%	2020	(12)
14.	Fenofibrate	Copovidone (K28), Aerosil 200	1:17	Hot-melt extrusion	20%	2020	(13)
15.	Cyclosporine	Hydroxypropylmethyl-cellulose acetate succinate	1:7	Hot-melt extrusion	50%	2015	(14)
16.	Indomethacin	HPMC	1:3	Hot-melt extrusion	60%	2014	(15)
17.	Felodipine	Hydroxypropyl cellulose	3:7	Hot-melt mixing	30%	2014	(16)
18.	Nimodipine	Kollidon VA64	3:37	Hot-melt extrusion	10%	2011	(17)

Table I (continued)

Sr. No.	API	Polymers	Percentage of drug: excipient	Preparation method	Increase in solubility relative to pure API	Year	Reference
19.	Ibuprofen	Eudragit® L100–55, polyvinyl alcohol (PVA-Mowiol4–88),	1:9	Freeze-drying	100%	2019	(18)
20.	Ascorbic acid	Polyvinylpyrrolidone (PVP, 40,000 MW), polyacrylic acid (PAA, 450,000 MW), food grade pectins	1:8	Freeze-drying	20%	2015	(19)
21.	Paclitaxel	Polyvinylpyrrolidone K30	1:9	Freeze-drying	41%	2013	(20)
22.	Atorvastatin	Triton WR 1339, double-toned milk (fat content 1.5%)	1:9	Freeze-drying	32%	2012	(21)
23.	Ezetimibe and Lovastatin	Soluplus1, Eudragit L1001 (poly (methacrylic acid-co-methyl methacrylate), and Eudragit L100–55	5:5:90	Spray-drying	25%	2017	(22)
24.	Docetaxel	Polyvinyl pyrrolidone K30 (povidone K30, PVPK30), Sodium dodecyl sulphate (SDS),	1:9	Spray-drying, freeze-drying	90%	2016	(23)
25.	Ziprasidone	(HPMCAS), Poloxamer 338 (Polysorbate 80) (Tween® 80), and Soybean lecithin	1:1.3	Spray-drying	80%	2012	(24)
26.	Clopidogrel	Hydroxypropylmethylcellulose (HPMC 2910), d-Mannitol, crospovidone, colloidal silica	11.069:3:3.5	Spray-drying	80%	2011	(25)
27.	Sibutramine	Gelatin and HPMC	1:0.8	Spray-drying	62%	2010	(26)
28.	Ferulic acid	Polyvinylpyrrolidone K30	15:30	Electrospinning	71%	2010	(27)
29.	Itraconazole	Aerosil® 200, microcrystalline cellulose, mannitol, PVPVA64, and Kollidon® CL	4:6	Electrospinning	85%	2016	(28)
30.	Ritonavir	Polyvinyl alcohol 4	3:1	KinetiSol dispersing	80%	2016	(29)
31.	Telmisartan	Soluplus, polyvinylpyrrolidone (PVP)	7:3	Physical mixing and grinding	70%	2013	(30)
32.	Vemurafenib	HPMCAS, HPMCP	1:8	Solvent-controlled coprecipitation	30%	2013	(31)
33.	Tadalafil	Pluronic F-127 (PF-127), pluronic F-77 (PF-77), pluronic F-68 (PF-68), pluronic F-38 (PF-38), and pluronic F-107 (PF-107)	1:5	Fusion method	50%	2010	(32)

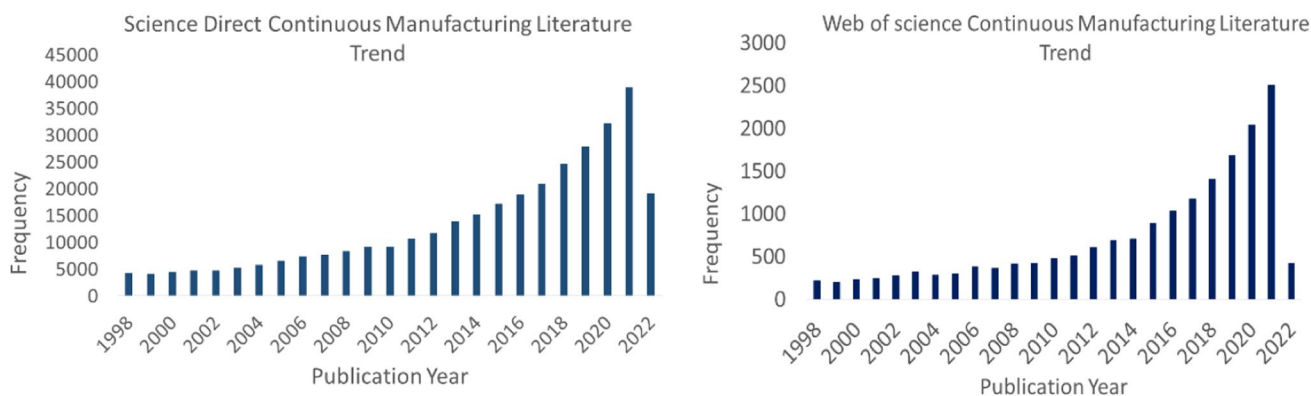


Fig. 4 Literature trend of “continuous manufacturing.” **a** Science Direct, **b** Web of Science

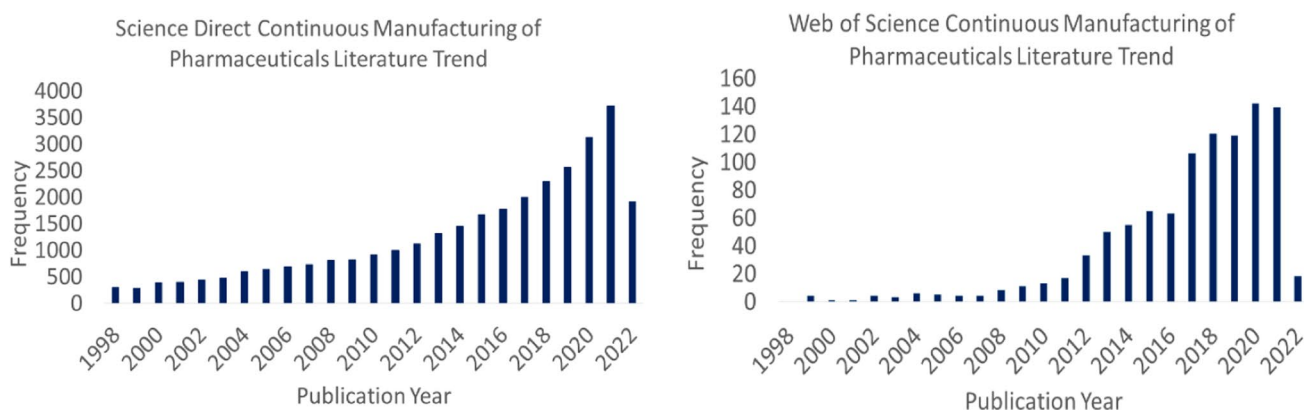


Fig. 5 Literature trend of “continuous manufacturing” in “pharmaceuticals.” **a** Science Direct, **b** Web of Science

scientific literature was observed, with exponential growth from 2017 onwards (Fig. 5), reflecting increasing adaptation of continuous processing in pharmaceutical manufacture.

Continuous Manufacturing for ASDs

Amorphous materials can be manufactured using processes that can be categorized into three different types: solvent evaporation, melt-cool, mechanical procedures using a ball mill, *etc.* The difference between batch and continuous manufacturing is illustrated in Fig. 6. Hot melt extrusion (89) and KinetiSol technology (19) currently appear to be the most promising techniques for continuous manufacturing of ASDs. HME is a stable technique that can enable the production of ASDs without the use of solvents. Additionally, HME is a continuous process that is easily expanded from a small-scale laboratory extruder to production-scale machinery. For research, validation, manufacture, and maintenance, this approach is thought to be cost-efficient. For example, Thiry *et al.* performed an experiment that explored HME as a continuous technique to create cyclodextrin inclusion

complexes in order to improve itraconazole’s solubility and dissolution rate (90). Similarly, Maniruzzaman *et al.* reported that the HME technique demonstrated its processing abilities to develop different solid dosage forms, like pellets, capsules, films, or tablets (91). KinetiSol is another technology that quickly converts the physical mix into a melted form and produces a uniform solid dispersion and can also be used for continuous manufacturing. Similarly, LaFontaine *et al.* prepared ASD of ritonavir-polyvinyl alcohol by KinetiSol technology (92). Gala and coworkers prepared the amorphous solid dispersions of abiraterone and hydroxypropyl beta cyclodextrin by KinetiSol technology (16). The physicochemical characteristics of the API and the polymers that can result in a product that is physically and thermally stable are the basis for the choice of an optimal technique for preparing ASDs(19, 93).

Continuous manufacturing methods are well suited to the production of active pharmaceutical components as well as the manufacture of final dosage forms. Ivacaftor, an API from Vertex Pharmaceuticals, has relatively poor dissolution characteristics and bioavailability in the crystalline

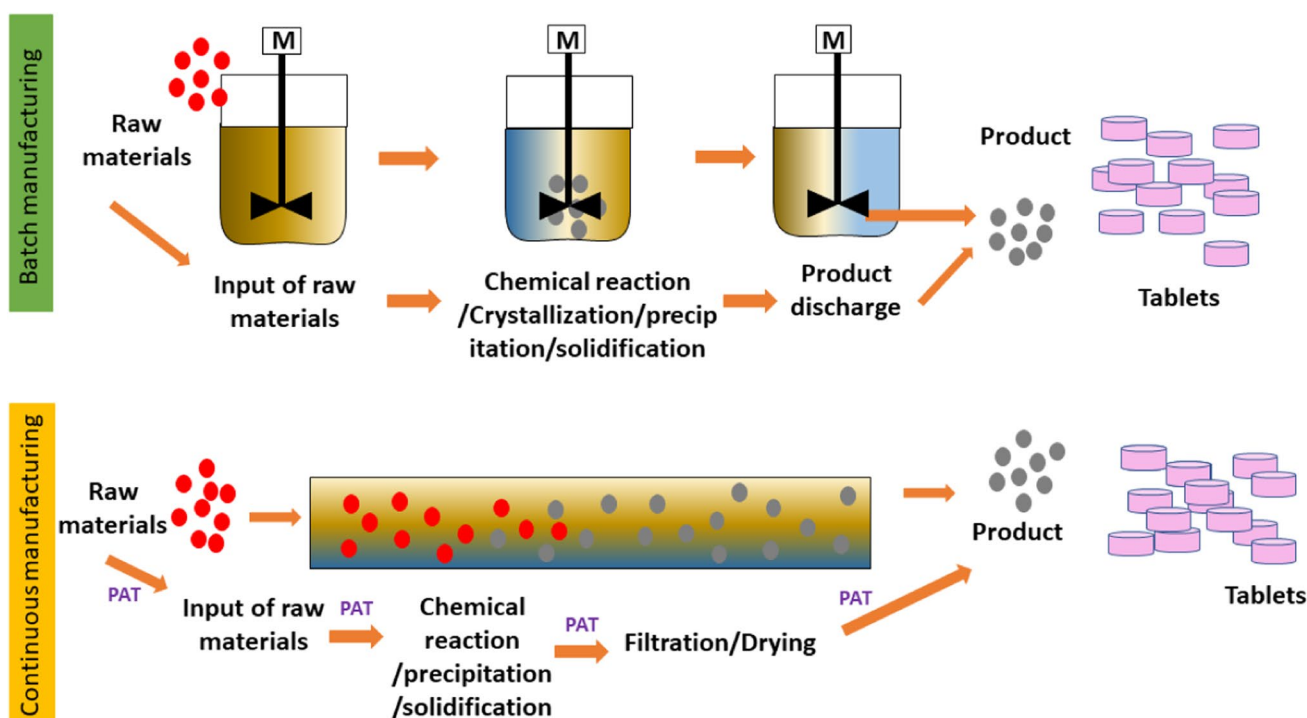


Fig. 6 Comparison between continuous manufacturing and batch manufacturing processes

form. Vertex generated ASDs of ivacaftor using both spray-drying and HME, which showed improved dissolution and oral bioavailability. Continuous manufacturing processes are suitable for ASDs due to high-quality criteria and good manufacturing practice norms. Several pharmaceutical companies have recently focused their attention on the continuous processing in pharmaceutical production. The FDA sees continuous processes as having a lot of potential since they can open new avenues for producing high-quality medicinal products. Increasing yields in production is a difficult task which can be achieved by continuous manufacturing techniques, where the manufacturing is controlled using artificial intelligence and PAT tools. Continuous manufacturing of drug-loaded ASDs also gives new possibilities for automation (94).

Hot-Melt Extrusion

Hot-melt extrusion (HME) is one of the most popular methods for manufacturing amorphous solid dispersions. In HME, an extruder feeds raw materials into an apparatus with one or two revolving screws that are heated to varying temperatures, after which the material is treated and fed through a die to generate the desired shape and size. Muvva *et al.* reported increased bioavailability of apremilast when processed by the HME method (95, 96). Similarly, Lee *et al.* also performed research on improving the solubility and bioavailability of rivaroxaban (RXB) which is poorly

water-soluble. They prepared RXB-containing hot-melt extruded ASD (HME-ASD) by altering the API: polymer (polyvinyl pyrrolidone-vinyl acetate 64) ratio and barrel temperature (1:1–1:4) (200–240°C). Solomon *et al.* worked on felodipine to form ASDs by the HME process without the use of a solvent (97). Emam *et al.* generated meloxicam ASD by HME, which resulted in an improvement in dissolution and bioavailability (98). Using HME technology, researchers built a microenvironment pH-modulated ASD system of telmisartan. The microenvironment pH adjustment produced by the inclusion of an alkalizer was one of the reasons for the improved solubility, bioavailability, better wettability, and increased drug release in a favorable pH environment (99). One-step co-extrusion as a continuous production process in ASD manufacture is growing rapidly in the industry and academia. In one study, Maniruzzaman *et al.* used magnesium alumina metasilicate as a carrier for continuous extrusion processing to create ASDs of indomethacin which showed enhanced solubility and dissolution rate. Under stability studies, the extruded solid dispersions displayed good flowability and physical properties without indomethacin crystallization or changes in physical stability (100). A one-step HME technique was used to successfully manufacture an ASD of nisoldipine with Kollidon VA64. It disintegrated faster when compared to commercial tablets and their physical mixture (101). These examples show that the process of one-step extrusion will likely be more useful than other commonly used technologies like

spray-drying, solvent evaporation method, and fluid bed technology method for continuous manufacturing of ASD-based formulations.

A predictive tool for the selection of various formulation components for ASDs in HME processes is based on Flory-Huggins thermodynamic modeling (102). The Flory-Huggins solution concept is a lattice model of the thermodynamics of mixing polymeric solutions. This theory provides a useful framework for creating an ASD design space (103). Moseson *et al.* used the Flory-Huggins-based model, where melting temperature depression measurement was used to create the phase diagram for indomethacin and polyvinylpyrrolidone/vinyl acetate copolymer (93). Suryvanshi *et al.* used this theory for the evaluation of Kollidon®SR matrix-mediated amorphous filament extrusion of norfloxacin prepared by HME (104). The Hildebrand and Scott solubility factor was calculated at 25°C, and the melting point depression of the drugs in polymer blend at the melting temperature was used to determine the Flory-Huggins (F-H) interaction parameter for the drug and polymer at varying temperatures which indicates enthalpic and entropic changes in solubility and defines the thermodynamic features of drug-polymer solutions. Numerous investigations have discovered that, within a small compositional range, fluctuates proportionally to the opposite of the melting point of the drug (105). The Flory-Huggin's theory of the fusion power of mixing allows for the entropic contributions of polymers and intraspecies interaction; however, the corrective entropy element provided by Hildebrand and Scott has been omitted in the computational techniques that are extensively used for calculations. Turpin *et al.* highlighted some of the novel *in silico* screening methods for ASD for troubleshooting solubility parameters, arguing for the adoption of PC-SAFT2 (perturbed-chain statistical associating fluid theory) (102).

Spray-Drying

Spray-drying is a drying method that can produce nano to micron-sized particles in a short period of time. Spray-dryers can turn crystalline starting materials into amorphous products. Ha *et al.* used spray-dried Eudragit E/HCl, which is a cationic polymer, to create an ASD of trans-resveratrol. The amorphous Eudragit E/HCl solid dispersion displayed supersaturation without precipitation for 48 h. The absolute oral bioavailability of trans-resveratrol solid dispersion was found to be increased (106). Mudie *et al.* manufactured spray-dried ASD for tablets and achieved improved bioavailability (107). Similarly, Costa *et al.* proved that spray-drying can be employed as a continuous manufacturing technique suited to the manufacture of ASD-based tablets, and they also stated that skipping the demixing step (API-carrier solubility), which is an alternative to prepared supersaturated API-polymer solid solutions by spray-drying, resulted in a

highly supersaturated liquid that delivered efavirenz from ASD formulations in seconds (108). Ziaee *et al.* prepared ibuprofen ASDs by spray-drying, and they indicated that it would be a suitable technique for continuous manufacturing of ASDs. The ASD gave a higher dissolution rate and solubility profile for ibuprofen than the crystalline drug (109). ASDs of dutasteride were prepared by spray-drying, and the link between supersaturation behavior assessed during dissolution and *in vivo* absorption improvement was evaluated (110). Raloxifene ASD nanoparticles were successfully generated by spray-drying aqueous solutions, demonstrating a case of green manufacturing as no organic solvents were used or produced in the process (111). The increase in the dissolution rate through the dextrin-based polymer dispersion system, the bioavailability enhancement, and the permeability enhancement by inclusion of SLS resulted in a considerable increase in oral absorption of amlodipine-free base ASD (18). Rivaroxaban-polymer ASDs have shown higher biopharmaceutical efficiency, including solubility and dissolution rate, than crystalline API in a pharmacokinetic trial with *in vitro* permeability analysis (112). With these examples, it may be reasonably expected that ASDs of other APIs could also be manufactured by spray-drying and that spray drying could be employed in continuous processing of ASDs.

Electrospraying Technology

The electrospraying technique is a relatively new method for producing ASDs. A solution of API and the inert polymer is gently forced through a nozzle to make solid dispersions *via* electrospraying. The liquid stream becomes highly charged when a high voltage is applied to the nozzle, generating electrostatic stress inside the fluid leaving the nozzle. The electric forces will counteract the surface tension of the liquid when there is enough electric potential between the vessel and the nozzle. A Taylor cone is formed when the meniscus of a liquid drop developing at the nozzle tip deflects into a conical shape. The free surface charges are accelerated and concentrated at the cone's tip, resulting in the generation of a jet that accelerates downwards before breaking up into droplets, and has a high potential for continuous manufacturing. This technique allows fine-tuning of powder morphological properties and API release characteristics. Smeets *et al.* explained the utility of electrospraying for the creation of a fixed-dose combination product containing three APIs. Smeets *et al.* also studied the feasibility of coaxial electrospraying for the creation of gastro-resistant microparticles of darunavir ASD-based formulations. The formulation of darunavir had a burst release, and the API was readily available for dissolution (113). Although researchers have shown that electrospraying can successfully generate ASDs, there have also been reports highlighting the difficulty of

electrospraying in the preparation of ASDs. Mohammadi *et al.* discovered that when clarithromycin ASDs were generated by electrospraying, the medication was only partially amorphized. Similarly, Zhang *et al.* generated ASDs, which showed significantly improved drug release; however, partial amorphization was detected in the formulation. Apart from the API characteristics, one of the elements that cause inadequate amorphization during electrospraying is the ambient pressure (114). Using coaxial electrospraying, which allows for the generation of highly monodisperse droplets, reducing the number of satellite droplets, a solid core-shell solid dispersion was generated to solve the problem of the low solubility of fenofibrate. Dissolution and gastrointestinal absorption behaviors were greatly improved by the reduction in particle size as well as improvement in dispersion efficiency (115). Electrospraying should be explored further as a general amorphization technology, as it has been demonstrated to be favorable for the amorphization of ketoprofen and many other APIs which cannot be prepared from other methods, which are thermally labile (116). Different polymers typically employed in the formation of solid dispersions have been studied with electrospraying technology and the impact of process variables evaluated. The experiments have assessed the significance of experimental parameters such as the electric potential differential, flow rate, and nozzle tip to collector distance. The nature of the solvent and the quantity of polymeric solutions, concentration, and viscosity are recognized as critical formulation characteristics. This information is critical for rationally designing future electrospraying technologies for creating ASDs (116).

Coprecipitation Method

Coprecipitation means that the API and polymer must quickly shift from one solvent environment to another. In the first environment with a common solvent, both API and the polymer are soluble; however, in the second environment, both are insoluble (common anti-solvent). The polymer-API solid dispersion in the slurry must also be in a glassy state, *i.e.*, the glass transition temperature of the amorphous mixture as plasticized by the anti-solvent environment must be higher than the precipitation temperature. Coprecipitation is the simultaneous precipitation of a normally soluble component (API-polymer) with a macro-component (solvent) from the same solution by forming a mixed composite by adsorption, occlusion, or mechanical entrapment. Sichen *et al.* produced a sorafenib ASD using coprecipitation technology. They showed that instant-release tablets manufactured using sorafenib ASD resulted in enhanced oral bioavailability (117). Duarte *et al.* prepared an ASD of carbamazepine, a weakly water-soluble drug with solubility restricted absorption, by a novel solvent-controlled precipitation (SCP) approach called microfluidization to form

carbamazepine-amorphous solid dispersions (118). The production of indomethacin-ASD by coprecipitation was carried out by Lim *et al.* and co-workers, resulting in improved dissolution (119). A curcumin-CaCO₃ combination resulted in a significant increase in curcumin solubility when using the coprecipitation approach to create ASDs (120). An ASD formulated with a ratio of 1:10 diosgenin to Soluplus had enhanced solubility and stability. It was made *via* a coprecipitation technique, and the diosgenin-ASD showed a substantial increase in solubility (121). Wang *et al.* explained the process of coprecipitation where quercetin ASDs were successfully prepared when employing HPMCAS as a polymeric carrier (122). The coprecipitation-based tablets disintegrated reasonably slower than the spray-dried dispersion-based tablets in dissolution trials, but both attained the full release. The tablets showed comparable dissolution patterns.

PAT Tool-Assisted Continuous Manufacturing

The application of process analytical technology (PAT) in pharmaceutical manufacturing was initiated in 2004 by the US Food and Drug Administration (FDA). PAT supports the transition from batch to continuous manufacturing operations, and an increasing number of organizations are relying on it as a critical component of a real-time product release system. As a result, one of the many advantages that PAT may provide is a reduction in cycle time, faster process design, and faster response to market demand. PAT tools are the framework for designing, analyzing, and controlling production through timely measured data (*i.e.*, during processing) of essential quality and performance characteristics of raw materials, end products, and methods, with the aim of maintaining final product quality (123). PAT tools have primarily been used for the design, analysis, and control of diverse processes involved in production. PAT can be used to provide the necessary information on a range of parameters that could have a substantial impact on several critical quality attributes (CQA). PAT is effective for evaluating the physical and chemical quality of raw materials and finished products, which can lower engineering and production costs. PAT tools have enhanced operational control and amenability, which has led to continual and immediate improvements in product quality. PAT involves evaluating the level of quality at various intermediate (in- or out-line processing) stages and ensuring transfer of quality to the final product. This technology has become a revolutionary instrument in the industrial sector and is the subject of extensive research.

Continuous manufacturing is emerging as next-generation manufacturing and will be widely accepted by pharmaceutical industries with the help of advanced PAT tools (Fig. 7) (124). The key objectives of PAT tools are to improve process understanding and real-time quality monitoring (125). PAT techniques, such as spectral sensors and

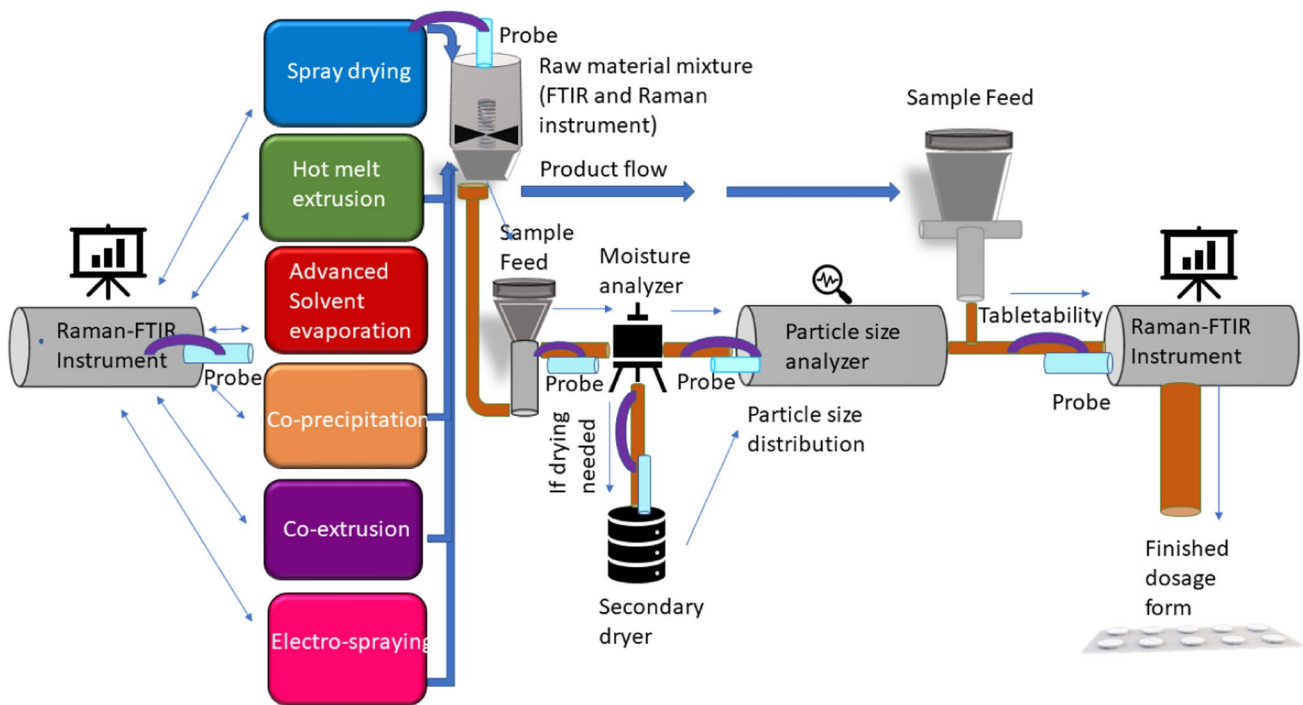


Fig. 7 PAT tools for continuous manufacturing of pharmaceuticals

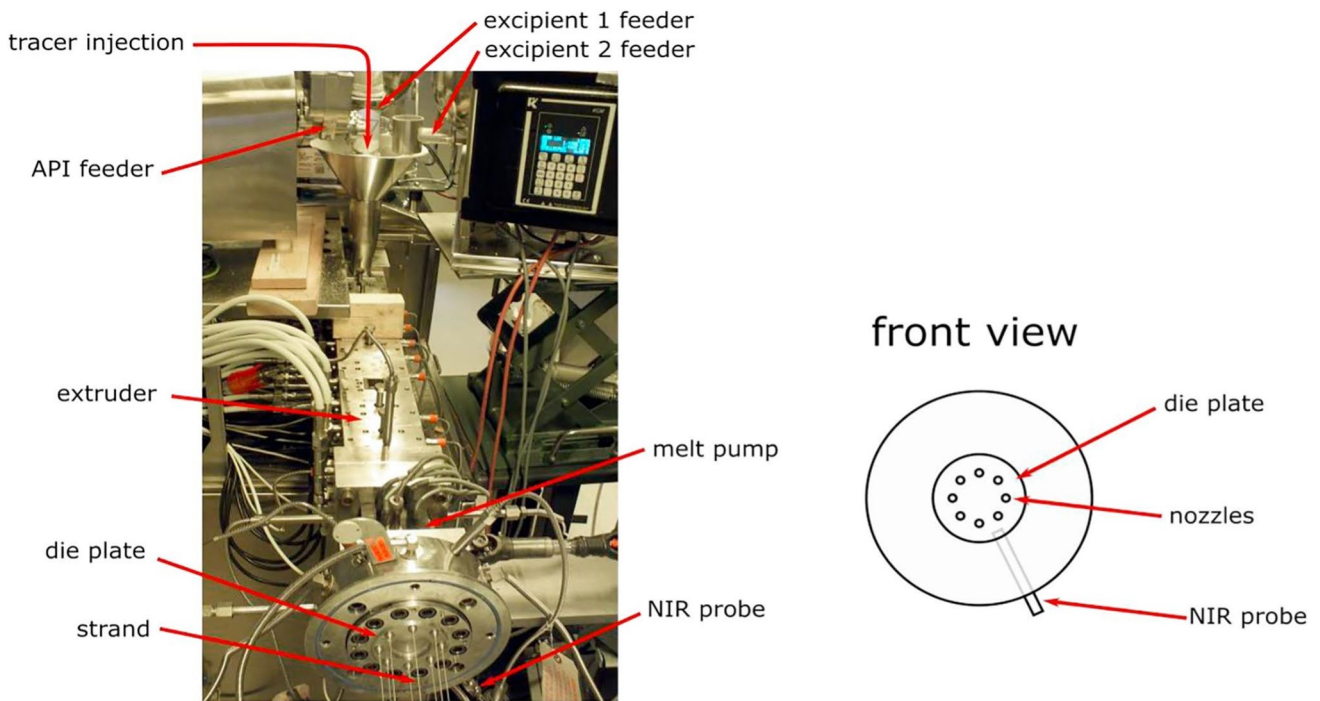


Fig. 8 NIR probe as PAT tool on hot melt extrusion (adapted with permission from (Khinast *et al*), Copyright Elsevier 2018)

chemometric models, are used to check product quality in real-time. In the pharmaceutical sector, as shown in Fig. 8 (126), near-infrared spectroscopy has been and continues

to be widely utilized to check product quality during continuous manufacturing procedures (123, 127). Similarly, Raman spectroscopy is also one of the PAT technologies

where method compatibility, validation, and convenience of use are all factors to consider when using Raman spectroscopy for pharmaceutical solids analysis. Fiber-optic probes are used in PAT Raman spectroscopy, with fiber designs with low separation between the activation and collection fibers (128). PAT tools make the process easier to monitor throughout, from raw material introduction to the finished products (Fig. 7). For example, in HME, in-line UV-Vis was employed as a quick PAT instrument to identify critical process parameters (CPPs) and their critical quality attributes (CQAs). A systematic strategy based on the continuous design of experiments was utilized to screen, optimize, and verify processing conditions using multivariable statistical analysis (CQAs) (129, 130). In the same way, Korasa *et al.* gave an overview of PAT in the monitoring of film coating unit operations (131). Galata *et al.* employed a PAT tool for monitoring continuous blending processes for tablets, including the steps of dry granulation (132), wet granulation (132), tableting (132, 133), and film coating (131). Chalbani *et al.* also incorporated NIR spectroscopy as a PAT tool for moisture content determination (134). Silva *et al.* used PAT tools for monitoring the coating of microspheres in a bench scale fluid bed dryer (135) and continuous manufacturing of tablets (136). Krier *et al.* developed PAT tools capable of monitoring four CQAs involved in implant manufacturing. PAT instruments, both in-line and off-line (using Raman imaging), offered great insights into the process and could be effectively integrated into a real-time release or expedited release strategy (137). A PAT system built on digital photography was utilized for continual blending processes with a colorful API (riboflavin, RI). It was shown that this method could measure the RI at levels as low as 0.05 w/w percent (138). The comparable UV/Vis imaging-based techniques can be utilized to gather real-time data on the product quality; therefore, the proposed system might develop into a PAT tool (139). Similarly, the design of a multivariate light induced fluorescence PAT tool for in-line quantification of pharmaceutical substances (140). Chavez *et al.* performed optimization of a pharmaceutical tablet formulation based on a design space approach and using vibrational spectroscopy as a PAT tool. The above examples shown how PAT can be used in the production of different pharmaceutical dosage forms and can also help in continuous manufacturing of amorphous solid dispersions. The potential use of PAT tools in ASD and final dosage form continuous manufacturing is shown in Figs. 7 and 8.

Medicines Commercially Available as ASDs

ASD-based formulations are commercially viable and have been shown to be well accepted in terms of safety. ASD manufacturing technologies such as HME or spray drying are ideal for continuous manufacturing if well assisted by the

necessary PAT tools. MICARDIS is a commercially marketed telmisartan product. Giri and his co-workers combined the API with Soluplus, 30–90% w/w, by a HME method. Giri and his colleagues used an ASD-based drug delivery strategy to improve telmisartan's solubility, dissolving, and pharmacokinetic properties, and thus, the dose could be reduced up to 5.34-fold (99). The extended-release tablet, Envarsus XR®, used in conjunction with other drugs to help prevent organ rejection in kidney transplant recipients, was prepared by melt extrusion technology, with different polymers at a 10% w/w drug loading (tacrolimus), and it is one of the marketed formulations in the form of amorphous solid dispersions (141). Table II summarizes the US Food and Drug Administration (FDA)-approved marketed products based on ASDs. There has been an increase in the number of ASDs under development and reaching the market over the last decade. Lynparza (olaparib), Belsomra (suvorexant), Mavyret (glecaprevir/pibrentasvir), Venclexta Viekira Pak (ombitasvir/paritaprevir/ritonavir), and Onmel (itraconazole) are all ASD-based formulations where the ASD is prepared by HME (142). Stivarga (regorafenib), Zepatier elbasvir/grazoprevir, Isoptin (verapamil), Kaletra (lopinavir/ritonavir), Orkambi (lumacaftor/ivacaftor), Zortress (everolimus), Prograf (tacrolimus), Intelence (etravirine), Eplclusa (sofosbuvir/velpatasvir), Harvoni (ledipasvir/sofosbuvir), Kalydeco (ivacaftor), and Incivek (**telaprevir**) are some examples of marketed formulations of ASDs prepared by spray drying (142). Zelboraf is an ASD-based formulation of vemurafenib where the ASD is prepared by solvent-antisolvent precipitation (142). These are some of the commercially available dosage forms of ASDs listed in Table II. According to the trend, the most frequently used preparation methods for ASDs in marketed products are HME and the spray-drying method.

Molecular Modeling For ASDs

Molecular modeling is a vast research field; the two most frequently applied elements of computational modeling are molecular docking and molecular dynamics simulations, both of which have proved critical in the rapid identification of prospects for *in vitro* and *in vivo* assessment, as shown in Fig. 9 (143).

Virtual screening using molecular docking identifies hit compounds with both the highest binding affinity and correct binding interactions. The lack of or incorrect simulation of receptors' flexibilities is sometimes a drawback (144). There have been simulations which are reported abnormal transit-time dispersion using multiple-trapping Monte Carlo methods. Monte Carlo algorithm makes use of multiple exponential allocation trapping. The findings of the simulations are the change from nondispersive to dispersive transients as a function of temperature is the result of repeated carrier

Table II Amorphous Solid Dispersion-Based Marketed Formulations (33)

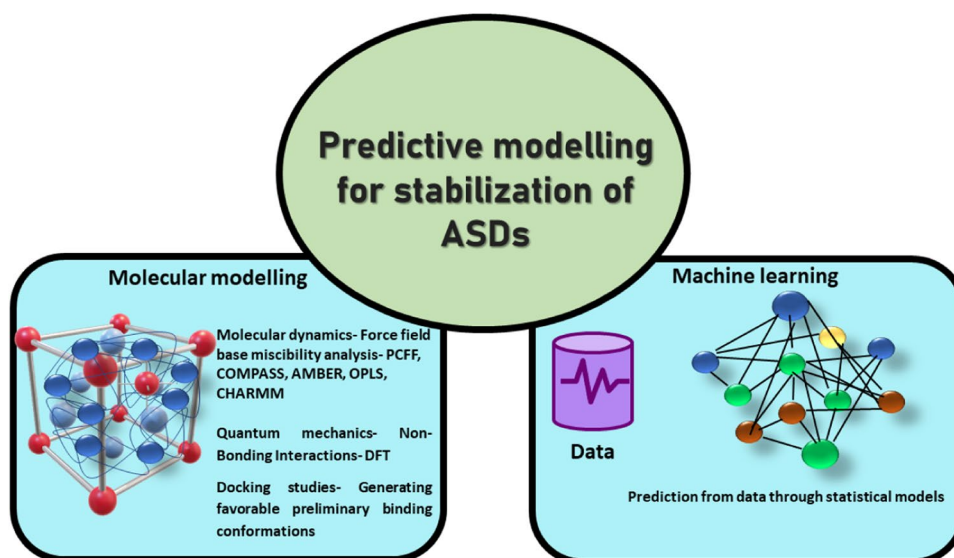
Sr. No.	Product name	Dosage form	Drug	Activity	BCS class	Preparation method	Year of approval
1	Lynparza®	Tablets	Olaparib	Ovarian cancer	IV	Melt extrusion	2018
2	Mavyret™	Tablets	Glecaprevir/pibrentasvir	Cancer	IV	Melt extrusion	2017
3	Venclexta®	Tablets	Venetoclax	Lymphocytic leukemia	IV	Melt extrusion	2016
4	Viekira XR™	Tablets	Ombitasvir/paritaprevir/ritonavir Dasabuvir	Hepatitis C	IV	Melt extrusion	2014
5	Belsomra®	Tablets	Suvorexant	Hepatitis C	II	Melt extrusion	2014
6	Noxafil®	Tablets	Posaconazole	Eczema	II	Melt extrusion	2013
7	Onmel®	Tablets	Itraconazole	Fungal infections	IV	Melt extrusion	2010
8	Norvir®	Tablets	Ritonavir	HIV/AIDS	II	Melt extrusion	2010
9	Kaletra®	Tablets	Lopinavir/Ritonavir	HIV/AIDS	IV	Melt extrusion	2007
10	Isoptin® SR	Capsules	Verapamil	Hypertension	II	Melt extrusion	1987
11	Stivarga®	Tablets	Regorafenib	Colon and rectal cancer	II	Spray drying	2017
12	Zepatier®	Tablets	Elbasvir/grazoprevir	Hepatitis C	II	Spray drying	2016
13	Orkambi®	Tablets	Lumacaftor/ivacaftor	Cystic fibrosis	II	Spray drying	2016
14	Epclusa®	Tablets	Sofosbuvir/velpatasvir	Hepatitis C	III	Spray drying	2016
15	Harvoni®	Tablets	Ledipasvir/sofosbuvir	Hepatitis C	II	Spray drying	2014
16	Kalydeco®	Oral granules	Ivacaftor	Cystic fibrosis	IV	Spray drying	2012
17	Incivek®	Tablets	Telaprevir	Hepatitis C	IV	Spray drying	2011
18	Zortress®	Tablets	Everolimus	Cancer	II	Spray drying	2010
19	Prograf®	Oral injections/capsules	Tacrolimus	Eczema	II	Spray drying	1994
20	Intelence®	Tablets	Etravirine	HIV	IV	Spray drying	2008
21	Astagraf XL®	Capsules	Tacrolimus	Hepatitis C	II	Wet granulation	2013
22	Rebagen®	Tablets	Rebamipide	Peptic and mouth ulcer	IV	Continuous spray Granulation	2013
23	Zelboraf®	Tablets	Vemurafenib	Melanoma	IV	Solvent/ antisolvent precipitation	2011

entrapment and disrupted surface release (145). The implementation of the Monte Carlo algorithm-based simulation of surface dynamics has criteria for choosing which atoms are permitted to be moved about during the simulation and for determining how many MMC cycles should pass before the simulation is terminated (146). Molecular modeling involves model building and computation to study molecular structure and functions. Modeling of molecular systems is often carried out through quantum mechanics (QM), molecular mechanics (MM), and hybrid QM/MM that describes molecular energies and geometries using cumulative physical forces. Molecular dynamics encompasses the observation of system behavior over time using molecular mechanics (147). Molecular dynamics is a significant computational tool for deducing the function of biological macromolecules, the physical basis of the structure, and the dynamic evolution

of the system (148). Molecular simulations have the potential to serve as a significant tool for the future development of ASDs as molecular modeling, when applied to ASDs, enables one to observe the microscopic interactions of the system and extrapolate them to macroscopic scales to better predict physical stability and phase separation. Thus, microscopic mechanisms can be associated with collective properties of the system (149–153).

In an ASD, the active pharmaceutical ingredient (API) dispersed in the polymeric carrier undergoes nonbonding interactions such as van der Waals, acid-base/ionic, dipole-dipole, and hydrogen bonding. These interactions are not only responsible for preventing self-association between like molecules but also play a significant role in promoting the physical stability of the ASD *via* enhancement in API-carrier interaction energy (154–156). Determining the

Fig. 9 Applications of modeling tools in ASDs



extent and types of such interactions helps understand the miscibility between the API and carriers.

Docking Studies

Docking studies are generally helpful in generating favorable preliminary binding confirmations between the API and the polymeric carrier in an ASD system. Molecular docking simulations help in more in-depth analysis and energy refinement of the constituents post rapid screening and scoring *via* docking studies (157). Fule *et al.* performed docking studies of the antimalarial lumefantrine and polymers Kollidon VA-64 and Soluplus. The docking results showed a strong hydrogen bond between the drug's hydroxyl, amine, and chlorine groups and the monomers of vinylpyrrolidone-vinyl acetate and Soluplus (158). Docking can also screen the stable tautomers before applying MD simulations. In one such study, Gangurde *et al.* used docking to analyze the binding energy of keto-enol and diketo forms of curcumin with Eudragit EPO. It was found that the diketo tautomer was more stable, with binding primarily being governed by van der Waal's forces. MD simulations were then applied after these docking studies, which afforded a more comprehensive structural insight into the interactions between curcumin-Eudragit EPO (159). Macháčková *et al.* undertook a detailed docking study wherein they performed systematic docking simulations with chitosan, L/D-poly lactide, PEG, polyglycolic acid, and cellulose with cyclosporin A. Each extensible polymer produced a million complexes with static cyclosporin A. Based on the binding energy, cellulose and chitosan were expected to be more miscible with cyclosporin A (160).

Molecular Dynamics (MD)

ASDs are large and complex systems, and studying such systems requires advanced tools. Molecular dynamics (MD) is a tool that facilitates the study of such phenomena from a more physically realistic point of view. The application of MD necessitates that all constituent components of the system are parametrized by a molecular mechanics-based force field assigning the system's total energy as a sum of empirical potential energy functions (potentials) (161). Force fields commonly applied to API-excipient ASD modeling include polymer consistent force field (PCFF) (17), condensed-phase optimized molecular potentials for atomistic simulation studies (COMPASS) (162, 163), assisted model building with energy refinement (AMBER) (164), optimized potential for liquid simulations (OPLS) (165), and chemistry at Harvard macromolecular mechanics (CHARMM) (166, 167). These force fields describe energy as dependent on atomic positions. The subcomponent potentials can be divided into those for bonded atoms accounting for bond lengths, angles, torsions, and nonbonded atoms describing van der Waals and Coulombic interactions (168, 169).

Using force field COMPASS, Gupta *et al.* demonstrated the ability of molecular modeling to simulate and predict solubility parameters. MD was used to study the miscibility of indomethacin in polyethylene oxide (PEO), glucose, and sucrose. MD simulations revealed that indomethacin was miscible with PEO, borderline miscible with sucrose, and immiscible with glucose (170). Employing CHARMM, miscibility parameters between ibuprofen and carbamazepine were evaluated in polymeric carriers polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol graft copolymer/polyethylene glycol. Strong molecular interactions were

observed between these components, which was confirmed by DSC and FTIR analysis (157). Kapourani *et al.* used PCFF to determine miscibility parameters between simvastatin and PVP, which were further verified by DSC and hot stage polarized microscopy (171).

Yani *et al.* utilized Hilderbrand and Hansen solubility parameters to investigate miscibility between the APIs and polymers. Before the preparation of ASDs, MD simulations predicted Hansen solubility parameters and calculated total hydrogen bond interaction energy and the average hydrogen bond lifetime per monomer between polymer functional groups and API. As per the predicted solubility, ASDs of fenofibrate/PVP-VA 64, ibuprofen/PVP-VA 64, and ibuprofen/Eudragit EPO were then manufactured using HME. The relative intermolecular interaction was predicted to be weakest for fenofibrate/PVP-VA 64. This result was further validated by the observed recrystallization of this system (172). Han *et al.* envisaged preparing a ternary ASD system comprising glipizide (API), PEG (polymeric carrier), and Tween 80 (surfactant). MD simulations were used to study ASD formation, dissolution, and molecular mobility (173). Razmimanesh *et al.* evaluated ASDs of gemcitabine as the API and chitosan as the polymeric carrier. MD simulations were used to investigate the effects of hydration on API loading efficiency with varying concentrations of API. The strongest molecular interactions and the maximum loading efficiency in simulated aqueous conditions were found to occur at the intermediate concentration (40%) of gemcitabine (174). Xiang *et al.* used MD simulations to study the effect of hydration on HPMC with the aim of investigating any alterations in its properties. It was found that increasing water fractions led to an enhanced structural relaxation and increased molecular mobility (175).

Barmpalexis *et al.* used docking models involving ibuprofen and carbamazepine interaction using mixtures of Soluplus, PEG polymer, and plasticizer which are the most stable forms. The miscibility of the system was evaluated by means of Hoftyzer-Van Krevelen and Hildebrand solubility parameters. The ternary systems were found to be miscible as per the calculated solubility parameters and DSC experiment results. In addition to this, FTIR spectroscopy was used to analyze the intermolecular interactions within the ASD system. Strong H-bonding which was observed between the carbamazepine primary amine group and the carbonyl and amide groups from docking and MD was further confirmed in this way (157).

Quantum Mechanics

Quantum mechanics (QM) methods can be used to study the API-carrier nonbonding interactions. Density functional theory (DFT) is one such computational modeling tool that may be used to study solid-state pharmaceutical compounds.

The nonbonding interactions that occur between the API and the polymeric carrier in an ASD can be studied using methods such as DFT, through which hypothesized molecular complexes can be directly constructed, and their associated interaction energy calculated. It is a rapid and powerful computational methodology that can identify ionic and strong hydrogen bonding interactions and predict the energy of model complexes (176). This pure QM approach produces a static snapshot while ASD modeling and therefore calls for adequate, sometimes manual, conformational space sampling. When applying DFT to large chemical systems, the calculation time can be drastically reduced by truncating the polymers to their monomeric and dimeric forms in the model systems. This permits a more systematic and detailed structural investigation of the ASD system. DFT applications are being used to study hydrogen bonding and charge interactions. A critical step toward ASD formulation and rational excipient screening is considering both of these parameters, whether relying on complexes formed between the API and carrier is comprehending the crucial interactions which determine ASD stabilization and solubilization (177). In one such study to understand these interactions, Maniruzzaman *et al.* investigated the interactions between a cationic API and an anionic polymeric carrier (91, 178).

Nie *et al.* probed the molecular interactions between the anti-leprotic drug, clofazimine, and the polymeric carrier, hypromellose phthalate, in an ASD system. Potential strong donors and acceptors were identified using partial charge analysis. DFT geometry and energy calculations utilized a truncated model system with acetic acid as a structural substitution for hypromellose phthalate carboxylic acid. Based on the results of the calculations and spectroscopic studies, it was proposed that the formation of an ion-pair complex is crucial for API-carrier miscibility (179).

DFT calculations have also been used to predict ASD storage stability. Wang *et al.* investigated the ability of polyvinyl pyrrolidone (PVP) to inhibit the crystallization of PVP-griseofulvin and PVP-resveratrol ASDs. DFT calculations and FTIR spectroscopy were used to investigate the relative interaction strengths between API-API and API-polymer complexes. Greater stabilizing hydrogen bond interactions were found to occur between the PVP-resveratrol ASDs as compared to PVP-griseofulvin ASD. The stronger interaction energy between PVP and resveratrol was found to be the contributing factor to the storage stability of the ASD and also yielded a continuous high dissolution rate of up to 90 days of storage, whereas a lower dissolution rate was observed for the PVP-griseofulvin system (180).

Machine Learning for ASDs from Molecular Modeling

Machine learning (ML) is increasingly being used in several aspects of the pharmaceutical sector, including drug

development, allowing the industry to grow as a whole (181). Machine learning capabilities and their utility in drug development and simulations are becoming important, so it is critical that ML be included in future breakthroughs in the field of ASDs. The inclusion of a novel drug molecule into a suitable pharmaceutical ASD with desirable delivery characteristics follows the development of the novel therapeutic molecule. In this case, artificial intelligence (AI) may be able to take over the role of the classic trial and error methods for product development (182). AI integration in manufacturing could be beneficial to pharmaceutical manufacturing and business (183). Quantitative structure-activity relationship (QSAR) modeling has been used to predict features such as adsorption, distribution, metabolism, elimination, and toxicity (ADMET) or compound oral bioavailability (184). The QSAR comparison cluster prediction approach requires structured similarity searching, in which a cluster of chemicals with similar systems to the test molecule is identified in the learning data set and utilized to construct a model that serves as the foundation for toxicological prediction. So, in this way, AI, ML, and QSAR can play a major role in the development of ASDs. The screening of suitable polymeric carriers when developing an ASD system of a poorly water-soluble drug is a tedious process that requires a huge amount of time, leading to high development times and slower progression to clinical trials. This time can be lessened by acquiring suitable knowledge about the behavior of ASD formation, dissolution, and subsequently drug release from the carrier matrix. This knowledge enables one to guide and streamline the choice of suitable excipient candidates for ASD formulation.

The mechanism of dissolution of the API is crucial to understand when designing an ASD. This mechanism can include either rapid dissolution, which results in a fluid phase that promotes the formation of crystalline or amorphous API nanostructures inside the polymer carrier, the progressive release of amorphous API-polymer compounds from the larger bulk ASD complex, or the subtle release of API-polymer, but gelation by water can cause crystalline API-polymer agglomerations to develop at the ASD-solvent interface (185), (186). Chan *et al.* investigated the formation and dissolution of ASDs composed of ibuprofen, PEG, PVP, and poloxamer 188 (P188) using MD simulations. The simulated annealing method was used to model ASD formation. This was followed by water immersion with the aim of investigating dissolution behavior. While smaller ASD particles displayed rapid dissolution, the dissolution of larger particles was found to be dependent on the polymer. API mobility was found to be higher within PEG and PVP polymers that led to API aggregation and consequently recrystallization of API, while P188 slowed API aggregation, thus better stability and dissolution (187). Jha *et al.* utilized MD simulations to study the intermolecular interactions and dissolution behavior of

ASDs comprising phenytoin, a poorly soluble API, and cellulose-type polymeric carriers. The phenytoin diffusion rate was analyzed by determining the variation in a water weight ratio in order to determine the dissolution behavior. As the water weight increased, the diffusion constants were found to increase exponentially (188).

Challenges for ASD-Based Formulations: Regulatory Constraints

ASDs have shown potential in the delivery of poorly water-soluble drugs. There was not much research on ASDs until 2010; however, the interest in ASD-based research has gained much attention since then. Our literature review revealed that ASDs had been used to deliver multiple drugs, including griseofulvin, verapamil, ritonavir, tacrolimus, troglitazone, antifungal agents (*e.g.*, itraconazole), and immunosuppressant agents (*e.g.*, cyclosporin A). Because the increased bioavailability of ASD is due to the increased energy of the amorphous form, this drug delivery strategy has several drawbacks in manufacturing and storage. The key challenges associated with ASDs are their physical instability during manufacturing and after manufacturing and their humidity and temperature sensitivity/susceptibility, which impacts storage lifetime, although the type of packaging employed can reduce the risk of water uptake and crystallization.

Although our understanding has progressed dramatically in recent years, there are still numerous unanswered problems associated with ASDs. More research is needed to improve the predictability of ASD's unique physical and chemical properties and *in vivo* performance, including the molecular interactions between the drug and the polymer carrier.

The HME process to produce ASDs is gaining popularity in pharmaceutical companies, despite the fact that more than half of all polymer-carriers lack a temperature range (defined by thermal plus elastomeric properties) suited to using HME. Furthermore, several polymer-carriers have wide temperature ranges, which could make it difficult to process thermolabile APIs continuously (189).

Similarly, spray-drying has been recognized as one of the valuable methods to generate ASDs. However, it is a multi-step process. The spray-drying process entails: (1) a solvent system is used to dissolve the drug and inactive ingredients; (2) pumping the concentrated solution into the spray nozzle; (3) atomizing the solution flow into fine droplets through an external unit; (4) drying the fine droplets inside a drying chamber; and (5) dividing and accumulating the dried particles *via* an appropriate collector. Screening with milligram amounts of API has been made possible by miniaturized spray-dryers. Many experiments have shown that ASDs produced by small-scale or lab-scale spray-driers could be replicated at a bigger scale. The spray-drying technique for

amorphization of a low T_g drug has limitations because of the requirement to keep the output temperature low (below 35°C). For example, Shetty *et al.* prepared ASDs of ciprofloxacin by spray drying and found the outlet temperature to affect the degree of crystallization and also aerosol performance for pulmonary drug delivery (190). Similarly, Mangal *et al.* prepared ASDs based on colistin on the surfaces of colistin-meropenem co-sprayed particulates. This has been attributed to an increase in particle porosity in conjunction with an increase in colistin concentration, resulting in a reduction in meropenem co-sprayed particulate. Any ASD that becomes physically unstable when exposed to humidity because of porosity it should be carefully packaged or protected from moisture (191).

The use of pharmaceutical ASDs will be hastened further if a technological breakthrough delivers a scaled miniaturized solvent-free equipment, such as HME or KinetiSol technology, which allows for the assessment of solvent-free ASDs utilizing milligram quantities of API. For some APIs, the introduction of new polymer, like Soluplus, has improved stability and dissolution profiles. ASD matrices of HPMCAS, which is a common polymer with high T_g and low hygroscopicity, were improved by the inclusion of Soluplus®. The choice of new, unproven additives is a regulatory and policy decision as well as a pharmacologic safety risk. In respect of patent protection, pioneers of new polymers suitable for ASDs have a significant advantage. Nevertheless, gaining regulatory approval for novel excipients requires a significant amount of time and money.

In the case of ASD-based formulations, unfortunately, devitrification can occur during storage. Since the product may be subject to change during storage, it needs to satisfy regulatory requirements such as solubility and crystallization tendencies.

Quality by design (QbD) is a platform in which quality is determined by the finished product instead of quality control quantitative assays. By leveraging new technology and computational tools, critical quality attributes (CQA) are employed in QbD to analyze, regulate, and monitor essential manufacturing operations (by multivariate analysis). To obtain a product with the critical quality attributes (CQAs), QbD methods such as DoE and PAT are frequently used, which helps to discover the optimal design space of critical material attributes (CMAs) and critical process parameters (CPPs). The essential nature of these critical attributes in the drug products is based on their identification and screening. The use of a risk assessment tool as a QbD approach is commonly used to achieve this criticality (192). Multivariate analysis approaches are used to detect, classify, and measure statistically relevant variable effects on essential product qualities (193). The design and development of formulations and manufacturing procedures that ensure pre-defined product characteristics are all part of the QbD strategy. A QbD

approach based on the factorial design of experiments (DoE) was used to successfully develop a Carbopol 940 topical gel containing an aceclofenac-crospovidone ASD (194). QbD was also used to optimize the solid dispersion formulation and process factors for polypeptide-k (PPK-SD) manufactured by spray-drying. The resulting product powder flow characteristics and yield were found to be greatly improved when the ratio of trehalose to PPK was raised (195). In order to improve the dissolution rate and solubility of the poorly water-soluble drug efavirenz, QbD methods were used to produce and optimize an ASD (196).

Current Scenario

The present regulatory framework is supportive of advances in scientific research, which includes deserting old-style manufacturing processes in favor of dynamic continuous manufacturing. Regulatory authorities are encouraging manufacturers to embrace new technologies, as represented by ICH Q3, Q7, Q8 (R2), Q9, Q10, and Q11, and the introduction of QbD concepts, emphasizing science as well as risk-based methods to ensure product quality (197).

As the API and non-active component(s) do not exist in the same crystal lattice and often do not require stoichiometry, ASDs differ from salts and solvates. A quasi component is a non-covalently attached component, including a carrier, additive, or other excipients, that is added to the ASD to enhance properties. The co-processed API may not be deemed a new API according to FDA guidelines for industry, Regulatory Classification of Pharmaceuticals. It is crucial to define an ASD as an effective dosage form since it clarifies that all these materials are not in-process materials, an API mixture, or an active pharmaceutical intermediate. The alternative categorization of an ASD intermediate would have ramifications for both expiry dating and GMP production, posing major barriers to commercialization. Through a scientific-technical advice (STA) request, an input on continuous manufacturing techniques for a future phase 1 clinical study was recently received, from the Federal Agency for Medicines and Health Products (FAMHP) of Belgium: "From a regulatory standpoint, the Agency agrees with the Applicant's proposal to consider continuous manufacturing as a drug substance because it is regarded as vital for the (physical) convergence of amorphous form of the drug molecule, and thus its bioavailability and clinical outcomes." While the approach has certain flaws, it is a potential first step that could pave the door for broader adoption of continuous production (193).

Regulatory Harmonization and Convergence

To reach the quality target profile, the requirement for an ASD formulation, a complicated composition, should be

adequately justified, and this should be done from a clinical perspective: to enhance the bioavailability, physical stability, and pharmacological burden and strengthen the product's actual safety profile. The application of this type of formulation is to enhance the efficacy of the drug. In the case of inactive ingredients, only those that are generally regarded as safe (GRAS) are established for human use at precise doses are listed in the FDA's inactive ingredient registry. A full pharmacology study, including carcinogenic effects and chronic toxicity, is required to ensure that all necessary excipients are suitable for use in humans. This is particularly true in ASD-based formulations, where polymer quantities are often much higher than in traditional dosage forms. All types of equipment used in pharmaceutical ASD manufacturing must meet GMP guidelines and validation standards. The surfaces that come into direct touch with the finished product must comply with GMP guidelines. The regulatory guideline states that "the level of pertinent scientific knowledge given in the application for registration determines the degree of regulatory flexibility." Science- and risk-based filings and regulatory evaluations are based on the information gained and provided to authorities. All of the aforementioned guidelines, as well as the recently emphasized QbD framework, have the potential to make a substantial impact on the creation, optimization, and deployment of continuous manufacturing processes.

Conclusion and Future Perspective

The increasing number of drugs with low aqueous solubility, poor dissolution, and poor oral bioavailability remains an unresolved issue that needs to be addressed with suitable interventions. Many potential drug candidates are aborted in the developmental pipeline as they are unable to exert their therapeutic benefit due to poor solubility. This obstacle of insolubilization can be overcome by employing suitable formulation strategies, and ASD is one such strategy that can help enhance the solubility and dissolution rate of poorly soluble drugs. Although the technology of ASD has come a long way since its advent more than half a century ago, it has not yet been utilized to its full potential in the best possible manner. The problems that exist today with ASDs include screening, stability, and scale-up issues, which may be overcome by employing computational molecular modeling tools and continuous manufacturing techniques. For large dosage drugs, direct compression-based continuous manufacturing holds a lot of potential, and amorphous solid dispersions will play a significant role in that process. However, thorough investigations are necessary for amorphous material-based tablets as there is the possibility of crystallization, particularly at high compaction pressure. The chances of heterogeneous crystallization (on the surface or in the interior of the

amorphous material) exist, even at lower compaction pressure. Specialized 2D X-ray diffractometry techniques with high-intensity synchrotron radiation can be useful to detect phase transformation in tablets. Thakral *et al.* have provided detailed information on the compaction of amorphous APIs (198). To step further in this arena, a meticulous understanding of such concepts need to be attained. Further research in this field will enable the translation of preclinical evidence into clinical reality and bring more ASD-based formulations to the market.

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Authors Contribution Amritha G. Nambiar: conceptualization, literature survey, a compilation of data, and original draft writing. Maan Singh: writing, reviewing, and editing. Abhishek R Mali: writing, review, and editing. Dolores R. Serano: writing, editing, and reviewing. Rajnish Kumar: writing, editing, and reviewing. Anne Marie Healy: conceptualization, writing, editing, and reviewing. Ashish Kumar Agrawal: writing, editing, and reviewing. Dinesh Kumar: conceptualization, writing, editing, reviewing, overall modification, and correction. All authors have read and agreed to the published version of the manuscript.

Declarations

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